Appendices Appendix 1: Basic knowledge related to x-rays

1.1. The physics of x-rays

X-rays are wave-like forms of electromagnetic energy that are carried by photons. They are characterized by a wavelength comprised of between 0.03 nm and 10 nm, which means they fall between gamma radiation and ultraviolet light on the electromagnetic spectrum. The energy associated with X-ray is usually measured in electro-volts (eV). The shorter the wavelength of an electromagnetic wave is, the higher the energy of the associated photons. For example, visible light photons have an energy of around 2eV, while X-ray photons have energies between 30 to 150keV.¹

X-rays are classified as ionizing radiation, meaning they have the potential to interact with biological matter when they collide with it, altering its molecular bonds and producing ionisations. The process of ionisation (in which an electron is given enough energy to break away from an atom) releases energy that can damage living tissues.

There are three possible outcomes when X-rays encounter matter (Figure A1):²

- Transmission: once the X-ray beam hits an object it passes through it without any interaction, keeping the same direction and energy.
- Diffusion/Scattering: upon hitting the object, X-rays are reflected in different directions, without energy transfer, or with partial transfer of energy and induction of ionisation – a phenomenon known as the Compton effect.
- Absorption: the energy associated with X-ray is absorbed upon passing through an object, induction atomic ionisation – this is known as the photoelectric effect.

The production of images for medical applications is dependent on the Compton and Photoelectric effect of X-rays, which relies on ionisation and, therefore, has the potential to cause biological damage.



Figure A1: Main mechanisms of interaction between X-rays and matter.

1.2. X-ray production and image generation

X-ray generators (Figure A2) used in endovascular operating rooms rely on an electric current (characterized by a potential (kV)) to accelerate and induce electron collision on an anode. As much as 99% of the current's energy is transformed into heat, explaining the need for cooling systems in imaging equipment. The remaining 1% of energy is used to generate an X-ray beam that exits the X-ray tube.³



Figure A2: Example of an X-ray generator; electrons are accelerated (blue arrow) and collided on an anode (blue structure). Most of the energy is released in the form of heat, the remaining 1% forms X-rays.

The X-ray beam released travels through the operating table and the patient. Part of the beam is redirected in random directions due to the Compton effect, which accounts for scattered radiation. A proportion of the beam crosses the patient, with part of its energy being absorbed (photoelectric effect) before reaching the detector. The differences in the amount of X-ray absorbed as it passes through the body results in variable attenuation and, therefore, heterogeneous intensity of the X-rays leaving the body. Production of radiological images is ren this phenomenon.

The beam generated by X-ray machines is composed of X-rays carrying various energies (Figure A3). "Soft" X-rays carry low energy photons and are rapidly stopped by matter (absorption), they will mostly induce ionisation and are not useful for producing images.³ "Hard" X-rays with high energy photons cross biological matter with minimal interaction also does not generate a radiological image. The "intermediate" X-rays, however, carry enough energy to allow part of the beam to cross the matter and reach the detector and the rest to be absorbed. This is the fraction of the X-ray beam that will produce images.



Figure A3: Differences between the X-rays produced in a generator and their role in producing an image.

Spectral filters, usually made of aluminium or copper, are positioned at the exit of the X-ray generator tube and used to stop or attenuate the low energy "soft" X-rays. Without this, the image generated by the X-ray machine would be blurred.

The filtered X-ray beam directed towards the body crosses structures that have different densities. Once the uniform X-rays enters the patient, the range of densities of the structures it crosses results in a range of attenuation, thus transforming it into a heterogenous beam,⁴ that is registered as a characteristic image via the detectors (Figure A4).



Figure A4: Image formation from the different densities of the structures crossed by the X-ray beam.

Appendix 2: Radiation exposures reported for endovascular procedures

Author	Y ea r	Groups	Imaging System	Number of patients	KAP (Gy.cm²)	CAK (mGy)	Dose to the operator (µSv)	Dose to the staff (µSv)
			Mobile C- arm (Flat panel)	13	55.5 ± 38.9 (17.0–152.0)	300 ± 200 (100–600)	-	-
De Ruiter ⁵	20 16		Fixed C-arm	7	$244.5 \pm 142.2 (47.4-409.5)$	820 ± 540 (100- 1600)	-	-
			Fixed C-arm (Hybrid room)	26	$\begin{array}{c} 157.0 \pm 120.4 \\ (25.9 418.0) \end{array}$	600 ± 400 (100- 1600)	-	-
Antoni	20	EVAS	Mobile C- arm	32	54 (IQR 42.1- 76.8)		-	-
ou ⁶	16	EVAR	Mobile C- arm	32	111 (IQR 75.3-157.4)		-	-
Macha do ⁷	20 16		Mobile C- arm	127	48 ± 32		-	-
Stansfi	20	Without preprocedure run through and brief	Fixed C-arm	61	225.11 (16.63- 1671.57)	-	-	-
eld ⁸ 16	16	With preprocedure run through and brief	Fixed C-arm	44	142.22 (20.98- 635.31)	-	-	-
Nyhei m ⁹	20 16		Fixed C-arm	80	234 (81–517)	-	-	-
Bacchi m Neto ¹⁰	20 16		Fixed C-arm	30	-	-	292.6 (88.4– 459.5) ¤	207.0 (73.6– 407.0) ¤
Disall	20	Standard dose protocol	Fixed C-arm	25	213.83 (IQR 123.99- 290.14)*	-	-	-
Dias	16	Low-dose protocol, Fusion imaging	Fixed C-arm	22	98.85 (IQR 83.63- 164.70)*	-	-	-
Attiga h ¹²	20 16		Fixed C-arm (Hybrid room)	65	23 ± 25	-	620 ± 620 H	$470 \pm 340 \ddagger$
El- Sayed ¹ ³	20 17		Fixed C-arm	6	82.8 (53.61- 144.3)	-	11 (4-74)	92 (43- 203) ‡
	20	Centre 1	Fixed C arres	74	77.96 ± 7.04	504.47 ± 55.07	-	-
Tuthill	17	Centre 2	Fixed C-arm	32	318.97 ± 57.97	1219.22 ± 296.48	-	-
		Centre 3		18	43.43 ± 9.94	218.09 ± 42.75	-	-

		Centre 4	Fixed C-arm	21	181.99 ± 21.41	983 ± 100.18	-	-
		Centre 5	(Hybrid room)	35	114.23 ± 13.90	790.86 ± 118.11	-	-
Stange	20		Fixed C-arm (Hybrid room)	25	-	581 (116.2- 2695.8)*	-	-
nberg ¹ 5	18		Fixed C-arm	52	-	1178.5 (174.9- 3351.1)*	-	-
		Baseline	Fixed C-arm	8	-	-	120 ± 70 ¤	-
Miller ¹	20	Use of live dosimeters	Fixed C-arm	5	-	-	190 ± 40 ¤	-
6	18		Fixed C-arm (Hybrid room)	5	-	-	30 ± 20¤	-
Ruffin	20		Fixed C-arm	25	337 (232– 609)*	1608 (933– 2770)*	-	-
0 ¹⁷	18		Fixed C-arm (Hybrid room)	25	157 (113– 212)*	884 (558– 1379)*	-	-
De Ruiter ¹ ⁸	20 18		Fixed C-arm (Hybrid room)	38	93.1 (63.5- 132.5)*	400 (300- 700)*	28¤	16¤
<u>Schaef</u> ers ¹⁹	20		Fixed C-arm (Hybrid room)	53	168.34 ± 146.92	-	-	-
	18		Mobile C- arm (Flat panel)	107	49.93 (± 38.06)	-	-	-
Ahma	20 18	Without Fusion	Fixed C-arm (Hybrid room)	47	32.19 (IQR 14.31– 49.42)*	-	-	-
d ²⁰		With Fusion	Fixed C-arm (Hybrid room)	105	23.44 (IQR 15.77– 51.44)*	-	-	-
Hiraok	20 18	Without Fusion	Fixed C-arm (Hybrid room)	62	-	880 ± 833	-	-
a ²¹		With Fusion	Fixed C-arm (Hybrid room)	81	-	768 ± 529	-	-
Maure	20	Without cloud-based fusion (Cydar)	Fixed C-arm (Hybrid room)	21	21.7 (8.9- 85.9)*	142 (61- 541)*	-	-
l ²²	18	With cloud-based fusion (Cydar)	Fixed C-arm (Hybrid room)	33	9.17 (6.83- 14.74)*	70 (45- 100)*	-	-
Hertau lt ²³	20 18		Fixed C-arm (Hybrid room)	85	14.7 (IQR 10.0-27.7)*	107 (IQR 68.0- 189.0)*	-	-
Ockert 24	20 18	EVAR	Mobile C- arm (Flat panel)	30	22.6*	139*	-	-

		EVAS	Mobile C- arm (Flat panel)	30	12.4*	67.7*	-	-
<u>Tzanis</u> 25	20 19		Not specified	17	124.3 (41.4- 627.1)*		4.7±1.4¤	
Schulz 26	20 19		Fixed C-arm (Hybrid room)	50	96.6 (±90.3)			
<u>Kaladj</u> i ²⁷	20 19	With cloud-based fusion (Therenva)	Mobile C- arm (Flat panel)	49	70.9 (± 48.2)			
-		Without fusion (historical cohort)	Mobile C- arm (Flat panel)	103	67.3 (± 74)			
Werm elink ²⁸	20 19		Fixed C-arm (Hybrid room)	77	43.3* (IQR 28.4-63.3)		13 to 45¤	
<u>Tenori</u> <u>o²⁹</u>	20 19		Fixed C-arm (Hybrid room)	24	105 (± 116)	373 (± 257)		
<u>Rehma</u> <u>n³⁰</u>	20 20		Mobile C- arm Fixed C-arm (Hybrid room)	78 208	168 (± 111) 82 (+75)			
	20 20	Patient specific rehearsal with virtual reality	Not specified	30	12* (2.9- 50.9)			
Våpen stad ³¹		No rehearsal	Not specified	30	13* (3.4- 31.5)			
Zurche <u>r³²</u>	20 20	Standard imaging protocol Restricted use of	Fixed C-arm Fixed C-arm	17 26	174 (±79)	795.8 (±371.5) 761.4		
<u>Tzanis</u> 33	20 20	angiography	Fixed C-arm	73	153.2*	<u>(±121.4)</u>		
Harbr on ³⁴	20 20		Fixed C-arm	81	75* (IQR 48- 148)			
Peters ³ 5	20 20	EVAR	Fixed C-arm (Hybrid room)	40	278* (IQR 254-348)			

		EVAS	Fixed C-arm (Hybrid room)	67	275* (IQR 240-326)		
<u>Martin</u> ez ³⁶	20 20		Mobile C- arm	42	61.5 (±42.4)		
<u>Tanta</u> wy ³⁷	20 20	Using CO2 and CEUS	Not specified	15		182* (±135)	
<u>Rial³⁸</u>	20 20		Mobile C- arm	165	80 (±58)	307 (±257)	
Doelar e ³⁹	20 20	Without Fusion	Fixed C-arm (Hybrid room)	41	139.8 (±186.8)	694.0 (±913.8)	
-		With Fusion		20	159.1 (±102.4)	810.7 (±496.7)	
Farah ⁴ ⁰	20 20			1 4 3	39.1 (0.1– 30.1)		
Haga ⁴¹	20 20		Fixed system	172	371.3 (± 186.0)	1101 (±540)	
<u>Kakko</u> <u>s</u> ⁴²	20 21		Mobile C- arm	48	26.8 (20.8- 38.1)		
<u>Efthy</u> miou ⁴³	20 21		Mobile C- arm	87	36.6* (2.0– 167.8)		

Table A1: Literature review of published dose reports after EVAR between 2016 and 2022. Results are reported in means with standard deviation (SD) or (*) in median with range, or interquartile range (IQR) if stated. ¤, Dose measurement above the lead protections; +, Dose to the anaesthesiologists; +. ALARA : As Low As reasonably Achievable; KAP: Kerma-Area Product; CAK: Cumulative Air-kerma; CEUS: Contrast-Enhanced UltraSound; EVAR: Endovascular Aortic aneurysm Repair; EVAS: Endovascular Aortic aneurysm Sealing.

Aut hor	Ye ar	Groups	Imaging System	Number of patients	KAP (Gy.cm ²)	CAK (mGy)	Dose to the operator (µSv)	Dose to the staff (µSv)
Kir	201		Fixed C-arm	16	601	4970	21.5	13.2
kwo od ⁴⁴	6		Fixed C-arm (Hybrid room)	25	372	2580	14.1	7.1
De	201		Fixed C-arm	15	873.8 ± 652.5 (129.7–2590)	6000 ± 4700 (800 - 18000)	-	-
Ruit er ⁵	6		Fixed C-arm (Hybrid room)	19	598.2 ± 318.5 (128.6–1362)	3700 ± 2500 (1000- 10000)	-	-
		Standard Dose protocol (FEVAR)	Fixed C-arm	36	283.24 (IQR 192.08- 499.57)*	-	-	-
Dias 11	201 6	Standard Dose protocol (BEVAR)	Fixed C-arm	23	638.91 (IQR 436.96- 1002.66)*	-	-	-
		Low Dose protocol and Fusion imaging (BEVAR)	Fixed C-arm	21	241.72 (IQR 140.44- 432.04)*	-	-	-
		Low Dose protocol and Fusion imaging (FEVAR)	Fixed C-arm	33	262.87 (IQR 202.98- 367.69)*	-	-	-
Atti	201	FEVAR	Fixed C-arm (Hybrid room)	25	39 ± 33	-	1020 ± 1530 H, 690 ± 460 H	-
2	6	BEVAR	Fixed C-arm (Hybrid room)	17	48 ± 38	-	1310 ± 1580H, 700 ± 650 [‡]	-
Wa	201	FEVAR	Fixed C-arm (Hybrid room)	91	-	4159 ± 2573	-	-
ng ⁴⁵	8	Fenestrate d cuff	Fixed C-arm (Hybrid room)	12	-	$\begin{array}{c} 6063 \pm \\ 3086 \end{array}$	-	-
De Ruit er ¹⁸	201 8		Fixed C-arm (Hybrid room)	24	384.8 (265.2- 522.3)*	2900 (2000- 3700)*	297¤	171¤
Ma nun ga ⁴⁶	201 8		Fixed C-arm (Hybrid room)	84	-	1097 (IQR 978-1426)*	-	-

Ruf fino ¹⁷	201 8		Fixed C-arm	25	567 (388– 779)*	2882 (2011– 4230)*	-	-
		FEVAR	Fixed C-arm (Hybrid room)	11	210*	1800*	120*¤	60*¤
Kir kwo od ⁴⁷	201 8	off the shelf FEVAR	Fixed C-arm (Hybrid room)	9	280*	2200*	220*¤	110*¤
		CMD	Fixed C-arm (Hybrid room)	60	370*	2950*	370*¤	210*¤
Sch anz er ⁴⁸	202 0	FEVAR		732	82.8 (±158.9)	2920 (±2987)		
		Fenestrate d cuff after failed EVAR		161	154.6 (±218.5)	4750 (±18,304)		
Har bro n ³⁴	202 0		Fixed C-arm	66	119* (IQR 85-209)			
<u>Jun</u> <u>eja⁴ 9</u>	202 0		Mobile C-arm	11		2160 (±930.0)		
<u>Tim</u> ara n ⁵⁰	202 0	With magnifica tion	Fixed C-arm (Hybrid room)	123		2458* (IQR 1706-3767)	266* (IQR 104- 583)¤	
		With digital zoom	Fixed C-arm (Hybrid room)	28		1382* (IQR 999-2045)	101* (IQR 34- 235)¤	
Sen ⁵	202 0		Fixed C-arm (Hybrid room)	334	182 (±96)	2100 (±1800)		
Ten orio 29	201 9		Fixed C-arm (Hybrid room)	85	174 (±101)	1134 (±815)		
<u>Doe</u> <u>lare</u> <u>39</u>	202 0		Fixed C-arm (Hybrid room)	37	91.5 (±348.4)	2337.2 (±1744.9)		

Table A2: Literature review of published dose reports after fenestrated or branched endovascular aortic aneurysm repair (F/BEVAR) between 2016 and 2022. Results are reported in means with standard deviation (SD) or (*) in median with range, or interquartile range (IQR) if stated. ¤, Dose measurement above the lead protections; ‡, Dose to the anaesthesiologists. ALARA: As Low As reasonably Achievable; KAP: Kerma-Area Product; CAK: Cumulative Air-kerma.

Author	Ye ar	Anatom ical Regions	Procedures	Imaging System	Numbe r of patients	KAP (Gy.cm²)	CAK (mGy)	Dose to the operator (µSv)	Dose to the staff (µSv)
Ruiz-	20			Fixed C-					
Cruces ⁵²	16	Iliac		arm	48	105.7			
		Femoro	Recanalizati	Fixed C-					
		popliteal	on	arm	57	83.9			

			Patients	Mobile &					
	20		treated in	Fixed C-		14.2 (±			
Maurel ⁵³	17	Iliac	2012	arm	653	18.9)			
			Patients	Mobile &		215(+			
			treated in	Fixed C-	0.01	37.6)			
			2015	arm	306		205 (*		
							285.6* (IOP		
Stonganh	20	Femoro		Fixed C			(IQK 152.7		
erg ¹⁵	18	nonliteal		arm	99		132.7-		
	10	popilicui		Fixed C-			106.0*	1	
				arm			(IQR		
				(Hybrid			82.5-		
				room)	35		163.5)		
Kostova									
Lefterova	20	Femoro		Mobile C-		67* (0.6-			
54	18	popliteal	PTA alone	arm	78	711)			
			PTA +		20	78* (2.3-			
			Stenting		20	237)			
			recanalizati		20	15** (3.3- 353)			
			Recanalizati		39	5557		1	
			on +			121* (3.0-			
			stenting		52	160)			
	20			Mobile C-		/		1	
Guillou ⁵⁵	18	Iliac	Serie n°1	arm	43	37.7	173.4		
				Fixed C-					
			Serie n°1	arm	100	50	252.9		
		Femoro		Mobile C-					
		popliteal	Serie n°1	arm	56	21.5	93.8		
			G · 01	Fixed C-	00	20.2	00.1		
		11: P	Serie n°1	arm	99	20.2	98.1		
		Illac &		Mobile C					
		nonliteal	Serie nº2	arm	24	194	66.6	0.2·15.3¤	0.9
		popilicui	Serie II 2	Fixed C-	21	17.1	00.0	0.2, 15.5	0.9
			Serie n°2	arm	76	24.2	125.8	0.3; 15.7¤	0.8
Goldswei	20	Aortoili				252.0			
g ⁵⁶	19	ac			3215	(±294.4)			
		Femoro				145.6			
	_	popliteal			7203	(±212.2)			
D 57	20	***		Mobile C-		43.5* (IQR			
Boc ³⁷	19	Iliac	Angioplasty	arm	37	28.6-8/.4)			
			Stenting		161	34.9** (IQK 32 5_01 2)			
	-		Angionlasty		101	52.5-71.2)			
		Femoro	, antegrade			5.9* (IOR			
		popliteal	approach		446	4.3-8.6)			
			Angioplasty						
			, retrograde			30.8* (IQR			
			approach		34	22.2-48.3)			
			Stenting,						
			antegrade		110	8.3* (IQR			
			approach		113	0.0-12.3)		<u> </u>	
			retrograde			56.9* (20.0			
			approach		7	93.7)			
Stahlberg	20		approuvii	Fixed C-	/	28.7* (IOR		+	
58	19	Iliac	With Fusion	arm	11	19.7-42.2)			
			Without			43.8* (IQR		1	
			Fusion		15	28.0-84.6)			

	20	Aortoili	Not		23.1* (37.0-			
Tzanis ²⁵	19	ac	specified	36	296.0)		4.4±3.6¤	
	20				14.4* (0.4–			
Farah ⁴⁰	20	Iliac		130	119.9)			
		Femoro			4.1* (0.1–			
		popliteal		117	146.8)			
	20		Fixed C-		14*; 21.52	237		
Mougin ⁵⁹	22	Iliac	arm	56	(±4.14)	(46)		
		Femoro			4*; 8.46			
		popliteal		123	(±1.60)	80 (14)		

Table A3: Literature review of published dose reports after endovascular repair of lower extremities arterial disease between 2016 and 2020. Results are reported in means with standard deviation (SD) or (*) in median with range, or interquartile range (IQR) if stated. ¤, Dose measurement above the lead protections. ALARA: As Low As reasonably Achievable; KAP: Kerma-Area Product; CAK: Cumulative Air-kerma.

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