

# Organs to cells and cells to organoids: the evolution of in vitro Central Nervous System modelling

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In Review

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DP, RP and BB contributed to the conception, writing and review of the manuscript

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### *Abstract*

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With one hundred billion neurons and one hundred trillion synapses, the human brain is not just the most complex organ in the human body, but has also been described as “the most complex thing in the universe”. The limited availability of human living brain tissue for the study of neurogenesis, neural processes and neurological disorders has resulted in more than a century-long strive from researchers worldwide to model the central nervous system (CNS) and dissect both its striking physiology and enigmatic pathophysiology. The invaluable knowledge gained with the use of animal models and post mortem human tissue remains limited to cross-species similarities and structural features, respectively. The advent of human induced pluripotent stem cell (hiPSC) and 3-D organoid technologies has revolutionised the approach to the study of human brain and CNS in vitro, presenting great potential for translational adoption in drug screening and regenerative medicine. We have surveyed more than one hundred years of research in CNS modelling and provide in this review an historical excursus of its evolution, from early neural tissue explants and organotypic cultures, to 2-D patient-derived cell monolayers, to the latest development of 3-D cerebral organoids. We have generated a comprehensive summary of CNS modelling techniques and approaches, protocol refinements throughout the course of decades and developments in the study of specific neuropathologies. Current limitations and caveats such as clonal variation, developmental stage, validation of pluripotency and chromosomal stability, functional assessment, reproducibility, accuracy and scalability of these models are also discussed.

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## 16 17 **Abstract**

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26 induced pluripotent stem cell (hiPSC) and 3-D organoid technologies has revolutionised the  
27 approach to the study of human brain and CNS *in vitro*, presenting great potential for disease  
28 modelling and translational adoption in drug screening and regenerative medicine, also  
29 contributing beneficially to clinical research. We have surveyed more than one hundred years  
30 of research in CNS modelling and provide in this review an historical excursus of its evolution,  
31 from early neural tissue explants and organotypic cultures, to 2-D patient-derived cell  
32 monolayers, to the latest development of 3-D cerebral organoids. We have generated a  
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37 scalability of these models are also discussed.

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39

## 40 **Keywords**

41 CNS; *in vitro* modelling; neural cell lines; hiPSC; 3-D organoids; human neurons; human glia;  
42 neurogenesis; neurological disorders; cerebral organoids; organotypic

## 43 **1. Introduction**

44 The study of neurogenesis (summarised in Figure 1), neural processes and neurological  
45 disorders is a very challenging science, as the brain is a uniquely complex organ and is largely  
46 inaccessible for experimental investigations in living humans, which is mostly limited to  
47 discarded post-surgical tissue samples or neuroimaging, transcranial magnetic stimulation and  
48 electroencephalography studies (Komssi and Kähkönen, 2006; Stan et al., 2006; Brammer,  
49 2009; Eyal et al., 2016).

50 While animal models have appreciably advanced the understanding of human brain  
51 development and neurodegenerative diseases, the inherent developmental, anatomical and  
52 physiological differences between the central nervous system (CNS) of animals and the human  
53 can add complexity to the interpretation of findings (Elston et al., 2001; DeFelipe et al., 2002;  
54 Roth and Dicke, 2005; Herculano-Houzel, 2009; Mohan et al., 2015). As such, the current  
55 understanding of human brain development has been limited to common features shared with  
56 other animal species (Kelava and Lancaster, 2016b). Although centuries of human *post mortem*  
57 tissue examinations have contributed to the fundamentals of modern neuroscience, allowing the  
58 study of specific features of the human brain, these tissues cannot be implemented in functional  
59 studies (Filis et al., 2010; Kelava and Lancaster, 2016a). Consequently, researchers have  
60 strived to develop and optimise *in vitro* neural culture systems for advancing the understanding  
61 of the functioning of the CNS and the underlying pathogenesis of neurological diseases.  
62 Animal models, *ex vivo* and *post mortem* tissues have been utilised in other areas of brain  
63 research.

64 The seminal work of the pioneering “fathers” of neuroscience and Nobel laureates, Santiago  
65 Ramón y Cajal and Camillo Golgi provided the foundations for investigating the intricacies of  
66 the human nervous system’s macro and micro anatomy (Ramón y Cajal, 1904; Golgi, 1906).  
67 In his published volumes, Santiago Ramón y Cajal artistically summarised his work describing  
68 the structure and organisation of the vertebrate nervous systems and discussed his theories  
69 including, amongst others, the “neuron doctrine”, the law of dynamic, functional or axipetal  
70 polarisation of electrical activity in neurons and his ideas on neurogenesis, neural plasticity and  
71 neuronal regeneration/degeneration (Ramón y Cajal, 1894; 1904; 1909; 1913). Since then,  
72 neuroscientists have strived on the wealth of knowledge inherited from Cajal and Golgi, who  
73 immensely contributed to the evolution of modern neuroscience over these centuries.

74 In this review, we present an evolutionary overview of CNS modelling through an historical  
75 excursus (Figure 2), starting from the origins of neural cell cultures from tissue explants and  
76 organotypic cultures, to cell monolayers, aggregates and ultimately leading to the generation  
77 of complex 3-dimensional (3-D) cultures such as cerebral organoids from patient-specific  
78 isolated cells, emphasising the growing excitement for the latter in the quest for the most  
79 representative human CNS model. A detailed discussion of these models would go beyond the  
80 scope of this review and it has been reported elsewhere (Chesselet and Carmichael, 2012;  
81 Dawson et al., 2018).

82

## 83 **2. Tissue explants and organotypic cultures**

84 The first *in vitro* nervous system culture was established by Ross Harrison in 1907, where frog  
85 embryo grafts consisting of pieces of medullary tubes were cultured as hanging drops in lymph.  
86 Although Harrison was able to observe neurite extensions and maintained the culture for up to  
87 four weeks, it was not possible to generate permanent specimens with intact nerve fibres  
88 (Harrison, 1907; 1910). Decades later, the first culture of intact CNS from chick embryos was  
89 established, permitting the recapitulation of the developing brain architecture *in vitro*, by  
90 displaying the formation of early retinal tissue (Hoadley, 1924; Waddington and Cohen, 1936).

91 The original long term culture (up to 143 days) of human fetal brains was established in 1946  
92 by Mary Jane Hogue by using the roller tube approach (Hogue, 1946; 1947). In 1951, Costero  
93 and Pomerat successfully cultured neurons obtained from the cerebral and cerebellar cortex  
94 explants of adult human brains, for up to five weeks, using Maximow's flying-drop (Costero  
95 and Pomerat, 1951).

96 The first CNS organotypic culture was pioneered by Bosquet and Meunier in 1962 using rat  
97 hypophysis (Bosquet and Meunier, 1962). In 1966, Crain cultured explants from embryonic  
98 rat spinal cord and ganglia on collagen coated glass demonstrating that grafted neural tissue  
99 possessed organotypic differentiation and bioelectric properties for electrophysiological  
100 studies (Crain, 1966). Since then, brain slices of several cerebral areas have been established  
101 as organotypic cultures, including the hippocampus, substantia nigra, locus coeruleus, striatum  
102 and basal forebrain (LaVail and Wolf, 1973; Whetsell et al., 1981; Knopfel et al., 1989;  
103 Ostergaard et al., 1995; Robertson et al., 1997).

104 Although tissue explants and organotypic slice cultures more accurately recapitulate the  
105 cerebral cytoarchitecture, they are difficult to acquire and cell specific functional studies are  
106 subject to severe limitations (Kelava and Lancaster, 2016b). For instance, the handling of  
107 organotypic preparations remains quite challenging with respect to preserving the sterility,  
108 viability and the cytoarchitecture of the tissues (Walsh et al., 2005). Additionally, cell  
109 maturation in culture may differ within the explanted tissues, with some cell types displaying  
110 a mature phenotype while others remain immature, being dependent on the age of the subject  
111 at the time of tissue collection (Gähwiler, 1981).

### 112 3. 2-D neural cell cultures

113 The improvement in the ability to maintain cell cultures for extended periods has enabled a  
114 range of isolated primary nerve cell cultures to be established, including hippocampal neurons  
115 derived from rat fetuses (Dotti et al., 1988), cortical, hippocampal, cerebellar and midbrain  
116 neurons from rat embryos (Brewer, 1995; Lingor et al., 1999), forebrain neurons of adult  
117 canaries (Goldman, 1990) and primary microglia from cerebral tissues of neonatal rats (Giulian  
118 and Baker, 1986). The generation of glial cell cultures, viable for several weeks, was also  
119 achieved as described in the seminal study by McCarthy and De Vellis; dissociated cerebral  
120 cortices of 1-2 days old rat pups brains were used to isolate primary astrocytes and  
121 oligodendrocytes that were devoid of any viable neuronal cell (McCarthy and de Vellis, 1980).

122 Culturing of primary neural cells, however, is hampered by a limited culture lifespan and the  
123 finite number of achievable passages with non-proliferating quiescent mature neurons (Gordon  
124 et al., 2013). To overcome this, the first neural stem cells (NSC) were isolated from rat  
125 forebrains in 1989, establishing a self-renewing line of multipotent progenitors with the  
126 plasticity to generate progenies of the main neuronal phenotypes (Temple, 1989).

127 In 1992, Reynold and Weiss demonstrated the presence of NSCs in the adult CNS of murine  
128 brains through the isolation of nestin expressing cells from the striata and inducing their  
129 differentiation into neurons and astrocytes *in vitro*, thereby establishing appropriate culture

130 conditions to demonstrate the functional attributes of these stem cells (Reynolds and Weiss,  
131 1992). The availability of NSCs facilitated the culture of neuronal or glial cells, without the  
132 need for complex and laborious isolations of the latter cells from whole explants (Gordon et  
133 al., 2013).

134 In parallel, the development of immortalised cell lines eliminated the need for multiple  
135 acquisitions of tissue for neural cell culturing. The first immortalised neuronal line was derived  
136 from lymph nodes, infiltrated bone marrow and liver tissue of children with neuroblastoma  
137 cancer; these cells were cultured *in vitro* for up to one year and were capable of differentiating  
138 into tissues resembling mature ganglion cells (Goldstein et al., 1964). However due to the  
139 clinical heterogeneity of neuroblastoma, cultured cells were characterised by morphological  
140 variability, and thus efforts were made to develop more defined cell lines and improve the  
141 longevity of cultures (Biedler et al., 1973). This led to the generation of the SK-N-SH  
142 neuroblastoma cell line from metastatic bone tumour (Biedler et al., 1973), which was further  
143 subcloned to establish the widely used SH-SY5Y neuroblastoma line (Biedler et al., 1978).

144 To induce cells to display a more neuronal phenotype, the culture environment can be  
145 manipulated by the addition of growth factors and signalling molecules such as retinoids and  
146 dibutyryl cAMP (Kuff and Fewell, 1980; Kovalevich and Langford, 2013); this is exemplified  
147 by the experiment conducted by Pahlaman *et al.* (1984), where neuroblastoma cells were  
148 exposed to retinoic acid to display a neuroblast-like phenotype expressing immature neuronal  
149 markers (Pahlman et al., 1984).

150 Other secondary immortalised cell lines developed for modelling neuronal cells include the  
151 mouse neuroblastoma Neuro-2a (LePage et al., 2005), PC12, a rat derived adrenal  
152 pheochromocytoma line (Greene and Tischler, 1976), the immortalised LUHMES cell line  
153 from human embryonic mesencephalic tissue and NT2 cells, a human neuronally committed  
154 teratoma derived line capable of differentiating into a mixed population of neuronal and glial  
155 cells under retinoic acid exposure (Pleasure and Lee, 1993; Coyle et al., 2011).

156 In neurobiology, the majority of primary neuronal tissue cultures is derived from animal  
157 sources, and as such, the techniques used to develop them suffered the same limitations of  
158 animal models, such as costs, ethical considerations, the obvious inter-species differences and  
159 the incorrect assumption that orthologous genes share similar functions in closely related living  
160 systems (Hartung, 2008; Gharib and Robinson-Rechavi, 2011; Ko and Frampton, 2016;  
161 Shipley et al., 2016). Moreover, the main concern with using immortalised cell lines for the  
162 study of neurobiology and for modelling neurological conditions, is that these cells contain  
163 genetic and metabolic abnormalities which may not represent a normal cell or those of human  
164 patients (Gordon et al., 2013; Carter and Shieh, 2015).

165 In 1999, Vescovi *et al.* established the first human multipotent NSCs derived from a 10.5-week  
166 embryonic diencephalon (Vescovi et al., 1999). The establishment of human NSCs opened  
167 exciting opportunities in neurobiology, since normal cells of human derivation, with self-  
168 renewing and long-term culturing capabilities, could be used for the generation of a multitude  
169 of functional neuronal and glial progenies for disease modelling and potential clinical  
170 applications (Carpenter et al., 1999; Jakel et al., 2004).

171 Although efforts for the successful long-term *in vitro* culturing of NSCs have been made (Sun  
172 et al., 2008), these cells were found to be incapable of accurately representing stem cells *in*  
173 *vivo*, due to their inability to recapitulate the entire range of neural lineages and hence brain  
174 development (Conti and Cattaneo, 2010; Kelava and Lancaster, 2016b).

175 More recently, multipotent neural cells were obtained by direct conversion of fibroblasts by  
176 the ectopic expression of *ASCL1*, *BRN2A* and *MYT1L* (Vierbuchen et al., 2010) or by the sole  
177 expression of *SOX2* (Ring et al., 2012). However, it is not clear to what extent the  
178 reprogrammed neural progenitors are capable of retaining epigenetic memory and the fidelity  
179 of the resemblance with neural progenitors is yet to be determined (Velasco et al., 2014).

#### 180 **4. Human Pluripotent stem cell-derived neural cultures**

181 The advent of human embryonic stem cells (ESC) in 1998 (Thomson et al., 1998) and then  
182 human induced pluripotent stem cells (iPSC) in 2007 (Takahashi et al., 2007), have provided  
183 exciting prospects in the field of neuroscience. The tremendous plasticity of these cells as an  
184 unlimited source of specific cell types, and their replicative capacity *in vitro*, rendered them  
185 the ideal candidate for neurodevelopmental studies. In particular, the possibility to generate  
186 neuronal cells directly from iPS cells derived from patients affected by a specific disorder  
187 provides an unprecedented opportunity to study the very phenotype of these diseases *in vitro*.  
188 Figure 3, summarises the different methods of derivation of iPSCs and the various  
189 characterisation criteria for qualifying as pluripotent cells.

190 The differentiation of ESCs *in vitro* reproduces with great fidelity the *in vivo* neuroectoderm  
191 formation (Wu et al., 2010), and indeed, neuronal cells were amongst the first lineages to be  
192 differentiated using PSC technology (Reubinoff et al., 2001; Zhang et al., 2001). This was first  
193 achieved using ESCs, by inducing their neuronal differentiation in spheroid-like aggregates of  
194 cells (called embryoid bodies, or EBs), cultured in serum-free conditions to selectively promote  
195 the growth of neural cells, which self-organised to form rosettes (Zhang et al., 2001). These  
196 rosettes generated structures reminiscent of neural tubes (Curchoe et al., 2012), organised as  
197 progenitor zones resembling the ventricular and subventricular zones with the presence of  
198 radial glia (Shi et al., 2012b; Edri et al., 2015).

199 Subsequent studies improved methodologies to differentiate ESCs to neural precursors in the  
200 complete absence of serum or growth factors (Ying et al., 2003). The combination of the  
201 embryoid body-derived rosette and the serum free media provided the foundation for the  
202 serum-free embryoid bodies culture, which in the presence of inductive signals, including Wnt  
203 and Nodal antagonists (*Dkk1* and *LeftyA*, respectively) and Sonic hedgehog could generate  
204 forebrain (telencephalic) precursors on poly-D-lysine/laminin/fibronectin coated dishes  
205 (Watanabe et al., 2005) and could be further differentiated into cortical neurons (Gaspard et  
206 al., 2008).

207 However, because ESCs are of embryonic origin, they are subjected to considerable ethical and  
208 practical issues. The development of iPSCs has since introduced an advantageous tool for the  
209 study of neurodevelopment and neuropathology; the possibility of generating ESC-like cells  
210 from adult somatic cells, not only circumvents issues related to ethics and sample acquisition,  
211 but also provides the advantage of developing pluripotent lines directly from diseased patients,  
212 and hence the study of neurobiology and neurological disorders accounting for genetic  
213 variations within a more heterogeneous cohort of relevant genotypes/phenotypes (Avior et al.,  
214 2016). In fact, the same differentiation protocols can be applied to the generation of iPSCs for  
215 the provision of neural progenitors and specific neural lineages (Mariani et al., 2012).

216 Several different PSC differentiation methods were developed, although these are highly  
217 variable and unpredictable due to undefined factors such as the use of neural inducing stromal  
218 feeder cells, the heterogeneous nature of embryoid bodies and inefficient methods for the  
219 selective survival of neural cells (Schwartz et al., 2008; Denham and Dottori, 2011).

220 The development of neuralization protocols for PSCs has been one of the main areas of  
221 investigation in neuroscience and it is being achieved by the improved understanding of the  
222 underlying signalling pathways involved, leading to the development of more efficient  
223 methodologies such as dual SMAD inhibition (Chambers et al., 2009). The dual SMAD  
224 inhibition was accomplished by using Noggin and the small molecule SB431542 to inhibit the  
225 NODAL/Activin, TGF- $\beta$  and Bone morphogenic protein (BMP) signalling, **thereby inhibiting**  
226 **the differentiation into cells with a non-neural fate** (Chambers et al., 2009; Pauklin and Vallier,  
227 2015). The dual SMAD inhibition method obviated the need for stromal cells and embryoid  
228 body based techniques and permitted the efficient generation of a broad repertoire of PSC-  
229 derived neural progenitors within shorter differentiation times **in adherent monolayer cultures**  
230 (Chambers et al., 2009). The dual SMAD inhibition method was further improved by the  
231 addition of a glycogen synthase kinase 3 (GSK3) inhibitor to induce Wnt signalling activation,  
232 yielding progenitors which matched the gene expression profiles of developing fetal brains,  
233 and with a broad range of regional differentiation phenotypes, from rostral-caudal to midbrain  
234 and dorso-ventral patterning of neural progenitors (Kirkeby et al., 2012). In another  
235 experiment, dual SMAD inhibition **was combined with retinoid signalling to enhance**  
236 differentiation of PSCs to cortical neurons (Shi et al., 2012b).

237 Lineage priming of PSCs to the neural lineage has also been achieved by the forced expression  
238 of the single transcription factor Neurogenin-2 (or NeuroD1) which yielded the generation of  
239 mature neurons **expressing glutamatergic receptors and forming spontaneous synaptic**  
240 **networks within two weeks from transfection** (Zhang et al., 2013). Another study demonstrated  
241 **that the forced synergistic expression of the transcription factors ASCL1 and DLX2 induced**  
242 **the differentiation of PSC to near pure GABAergic neurons** (Yang et al., 2017).

243 Another common differentiation protocol uses retinoic acid treatment on embryoid bodies for  
244 promoting commitment to the neural lineage (Schuldiner et al., 2001). In participation with  
245 FGF and Wnt, retinoic acid is a potent caudalizing factor of the neuroectoderm and is a  
246 differentiation-inducing molecule essential for the development of the neural crest and the  
247 generation of cortical neurons (Villanueva et al., 2002; Diez del Corral and Storey, 2004;  
248 Siegenthaler et al., 2009). Retinoic acid has been demonstrated to inhibit neural proliferation  
249 and promote neurogenesis by inhibiting the expression of genes that negatively regulate  
250 neuronal differentiation (such as Notch and Geminin), while promoting the expression of  
251 proneural and neurogenic genes (Janesick et al., 2015). **However, it is important to note that**  
252 **although retinoids play a fundamental regulatory role during neural tube formation, their**  
253 **function in neural development and axial patterning are strictly context, time and dose-**  
254 **dependent, and therefore it is crucial to include retinoids at an appropriate differentiation stage**  
255 **in cultures** (Maden, 2002).

## 256 **5. Monolayer cultures to organoids**

257 With the improvement of differentiation methods, culturing techniques have also been refined  
258 to introduce structural complexities that better recapitulate the *in vivo* development and  
259 cytoarchitecture. Availability of this technology has led to a tremendous interest from  
260 researchers worldwide, particularly from the prospective of generating more representative  
261 models of the human phenotype, and as a means to “replace, reduce and refine” the use of  
262 animal models (Sneddon et al., 2017). The culture substrate is as essential to neural cell culture  
263 as the use of appropriate inducing factors. In the CNS, extra cellular matrixes (ECM) are crucial  
264 for cell migration and differentiation, therefore *in vitro* substrates are fundamental for the  
265 preferred differentiation of NSCs and support of differentiated cells (Franco and Müller, 2011).



266 The best-described substrates used for the *in vitro* culture of neural cells (whether NSC or PSC-  
267 derived) are poly-L-ornithine, poly-L-lysine, fibronectin, collagen and laminin (Ge et al.,  
268 2015). All these substrates have been found to support neural differentiation to differing  
269 degrees (Ma et al., 2008). One study reports that poly-L-ornithine induces preferred  
270 differentiation of NSCs into neurons and oligodendrocytes, compared to poly-L-lysine and  
271 fibronectin (Ge et al., 2015). However, other studies suggested that laminin or laminin-rich  
272 substrates enhance differentiation of NSC to neurons (Hall et al., 2008; Ma et al., 2008).

273 Nevertheless, the ECM is a complex mixture of molecules (laminins, proteoglycans, collagens)  
274 and therefore specific combinations of substrates may be necessary to better reproduce the *in*  
275 *vivo* scenario (Ma et al., 2008; Franco and Müller, 2011). Hydrogel scaffolds such as Matrigel,  
276 which consist of a mixture of extracellular molecules including laminin, collagen IV, heparan  
277 sulfate proteoglycans and entactin (Kleinman and Martin, 2005) are often successfully  
278 employed for the culture and long-term support of neural cells (Ma et al., 2008; Lee et al.,  
279 2015). Matrigel is not only advantageous as a substrate for monolayer cultures, but due to its  
280 polymerizing nature, it can be utilised as a semi-solid scaffold matrix for 3-D cultures (Tibbitt  
281 and Anseth, 2009). However, even Matrigel is not immune from major limitations, being an  
282 animal-derived matrix characterised by batch variation and with an undefined composition that  
283 may produce a source of variability in experimental conditions (Hughes et al., 2010).

284 Traditional 2-dimensional (2-D) culturing has contributed immensely to the understanding of  
285 neuroscience but is substantially limited for recapitulating the *in vivo* complexities of the CNS.  
286 Advancement in cell culturing techniques for the generation of neural cell lines has greatly  
287 improved with the directed differentiation of iPSCs into monolayers of specific neural cell  
288 types (Pasca et al., 2014; Barral and Kurian, 2016; McKinney, 2017). A summary of various  
289 CNS neural tissues derived from the differentiation of iPSC is presented in Table 1.

290 However, these 2-D cultures are unlikely to recapitulate the intricate cytoarchitecture, the  
291 elaborate network of diverse neural cell types and the functional complexity of the *in vivo*  
292 central nervous system (Paşca, 2018). Cell differentiation and maturation is critically  
293 dependent on both intrinsic and extrinsic cues originating from the interactions with various  
294 neural cells and extracellular matrix molecules, and the cross-talk and dynamic interaction of  
295 neural cells is crucial for the recapitulation of a physiologically relevant system (Gomes et al.,  
296 2001; Rowitch and Kriegstein, 2010; Jiang and Nardelli, 2016).

297 Nevertheless, 2-D cultures have the advantage of a greater scalability, with less complex  
298 directed differentiation approaches and facilitated imaging. However, 2-D cells also favour  
299 stronger interactions with the surfaces of the culturing vessel rather than cell-cell interactions  
300 or between cells and the ECM, altering their proliferation and differentiation capabilities  
301 (Paşca, 2018). Three dimensional models can overcome 2-D culturing limitations, allowing the  
302 dynamic interactions between cells and ECMs and the recreation of signalling, metabolites and  
303 oxygen gradients across the culture (Ko and Frampton, 2016).

304 A variety of 3-D culture methods have been developed, with one example in the form of tissue  
305 explant cultures, such as whole brain sections grown in culture dishes or microfluidic devices  
306 (Ullrich et al., 2011; Huang et al., 2012).

307 For instance, recently, an organotypic human Alzheimer disease model consisting of a 3-D  
308 triculture system of neurons, astrocytes and microglia co-cultured in a microfluidic system was  
309 engineered. Authors developed this 3-D culture system to model the neuroinflammation and  
310 neurodegeneration aspects of the disease, employing human iPSC-derived neural stem cells  
311 overexpressing mutant *APP* and *PSEN1* genes associated with familial Alzheimer's. This

312 system successfully recapitulated the tauopathy,  $\beta$ -amyloid accumulation and microglia  
313 mediated neuroinflammation more efficiently than the 2-D models (Park et al., 2018).

314 However, these cultures are often problematic to maintain in the long-term and are generally  
315 derived from animal sources, and hence not representative of human development (Ko and  
316 Frampton, 2016). Self-organised aggregate cultures are an alternative 3-D *in vitro* culture  
317 approach, encompassing neural spheroids (Dingle et al., 2015). Further sophistication of  
318 culture methods has led to the modification of self-aggregating cultures for the generation of  
319 organ-like structures, termed organoids (Kelava and Lancaster, 2016b).

320 CNS organoids can be divided in two categories based on their patterning approach, either  
321 being self-patterned or extrinsically patterned. Self-patterned organoids are organoids that are  
322 cultured without the addition of exogenous morphogens that favour specific brain regions,  
323 whereas extrinsically patterned organoids refer to the generation of brain specific regional  
324 identities via the addition of morphogens and neurotrophic factors such as FGF, Sonic  
325 Hedgehog, Nodal, Wnt and BMP (Clevers, 2016; Brawner et al., 2017). Figure 3 illustrates the  
326 different brain regionals identities recapitulated in CNS organoids.

327 To illustrate this, the seminal study of Eiraku *et al.* demonstrated that serum-free embryoid  
328 bodies with quick reaggregation are capable of self-organising into stratified cortical tissues in  
329 cultures, thus showing that ESCs spontaneously differentiate toward a neural state by default  
330 (Eiraku et al., 2008). This notion provided the fundamentals to generate the first self-patterned  
331 CNS organoid, employing serum-free embryoid bodies to generate neuroepithelial cysts, which  
332 further self-organised into optic cup organoids, to present regions with retinal identities upon  
333 treatment with Nodal protein and culture on Matrigel basement membrane (Eiraku et al., 2011).

334 Extrinsic-patterning organoids can be exemplified by the generation of the first dorsal  
335 telencephalon organoid recapitulating a human cerebral cortex at 8-10-week gestation by  
336 Mariani *et al.*, where serum-free embryoid bodies were treated with Wnt and TGF- $\beta$  inhibitors  
337 and cultured on poly-L-ornithine, laminin and fibronectin for up to 70 days (Mariani et al.,  
338 2012). Similarly, other adaptations of the method developed by Eiraku *et al.* led to the  
339 generation of neocortical forebrain organoids maintained on Matrigel for over three months  
340 (Kadoshima et al., 2013). Further modifications of protocols for the generation of organoids  
341 patterned with other brain specific regions and sub-regions have been developed to model the  
342 adenohypophysis (using hedgehog agonists) (Suga et al., 2011), hypothalamus (by  
343 Nodal/Activin/TGF- $\beta$ , and BMP mediated inhibition) (Wataya et al., 2008), cerebellum (using  
344 the Nodal/Activin/TGF- $\beta$  inhibition and the addition of FGF2 and FGF19) (Muguruma et al.,  
345 2015), midbrain (by using the dual SMAD inhibition and Wnt activation) ((Jo et al., 2016) and  
346 hippocampal-choroid plexus (by treatment with BMP and Wnt) (Sakaguchi et al., 2015).  
347 Combining the strong neuralizing dual SMAD inhibition with the serum-free embryoid body  
348 approach also enabled the generation of cortical spheroids, which represented 3-D tissues  
349 containing neurons and astrocytes and mimicked cortical development stages up to the mid-  
350 fetal period (Pasca et al., 2015).

351 In 2013, Lancaster and Knoblich introduced, for the first time, the concept of whole-brain  
352 organoid or cerebral organoids (Figure 5), representing different brain regions within the same  
353 3-D platform. Cerebral organoids, are generated from PSC-derived serum-free embryoid  
354 bodies obtained by culturing in low concentrations of bFGF-2 and with ROCK inhibitors to  
355 promote cell survival (Lancaster and Knoblich, 2014). The serum-free embryoid bodies are  
356 subsequently induced to differentiate to the neuroectoderm within suspension cultures,  
357 establishing a radially organised neuroepithelium around the spheroid (Lancaster and  
358 Knoblich, 2014; Sutcliffe and Lancaster, 2017).

359 The resulting neurospheres are embedded into Matrigel hydrogel droplets, allowing the growth  
360 of continuous and orientated neuroepithelial buds and, the apicobasal expansion of the layer of  
361 neuroepithelial cells throughout the ECM basement scaffold. After the embedding, budding  
362 neuroepithelia generate fluid filled cavities reminiscent of ventricles. The neuroepithelium  
363 begins to migrate outwardly to generate the cortical layers consisting of Cajal-Retzius cells,  
364 deep and superficial cortical progenitors. On exposure to retinoic acid, cerebral organoids self-  
365 organise through self-patterning mechanisms to display sparse populations of neural  
366 progenitors including radial glia, which begin to expand forming cerebral structures (Lancaster  
367 and Knoblich, 2014). Retinoic acid is only added for terminal differentiation, as being a potent  
368 caudalizing factor it inhibits neurogenesis in the early stages of neuroepithelium formation  
369 (Petros et al., 2011).

370 The region in which radial glia originate, recapitulates the *in vivo* ventricular zone (VZ) and  
371 subventricular zone (SVZ) (Kelava and Lancaster, 2016a). Therefore, similar to *in vivo*  
372 neurogenesis, neural progenitors migrate to form the cortical plate, spontaneously giving rise  
373 to distinct brain regions reminiscent of the dorsal cortex, ventral forebrain, hindbrain, midbrain,  
374 retina, hippocampus and choroid plexus (Lancaster and Knoblich, 2014).

375 As cerebral organoids expand in culture, the neuronal population increases in number, resulting  
376 in the enlargement of tissues, reaching sizes of up to 4 mm in diameter (Sutcliffe and Lancaster,  
377 2017). The whole development process requires 7-10 days for the generation of neurospheres,  
378 and more than 20 days before the appearance of the first mature neural population (Lancaster  
379 and Knoblich, 2014; Sutcliffe and Lancaster, 2017). After one month in culture the cerebral  
380 tissue begins to thicken, showing tissues of different regional identities, as evidenced by the  
381 expression of FOXP1 (forebrain), TTR (choroid plexus), FZD9 (hippocampus) and SOX2 (VZ  
382 radial glia) (Lancaster and Knoblich, 2014). Later studies have confirmed that cerebral  
383 organoids display with high fidelity the gene expression signatures of a fetal developing  
384 neocortex (Camp et al., 2015).

385 The increase in size introduces problems with regard to nutrient and oxygen diffusion through  
386 the central regions of tissue, causing necrosis (Lancaster and Knoblich, 2014). Therefore, the  
387 organoids are grown in spinning bioreactors to provide agitation and maximise oxygen and  
388 nutrient exchange (Kelava and Lancaster, 2016b). Within bioreactors, cerebral organoids are  
389 capable of displaying a longevity of up to 1 year, although it has been reported that growth  
390 becomes stationary after 5 months, with organoids shrinking in size in subsequent months due  
391 to neuronal loss and disappearance of progenitors (Lancaster and Knoblich, 2014).

## 392 **6. Modelling neurological disorders with CNS organoids**

393 Since the generation of the first brain organoids, unsurprisingly, there has been an exponential  
394 surge in publications employing this technology (Figure 6), due to their amenability for the  
395 study of neurodevelopment and neurological diseases, but also as a potential platform for the  
396 development of novel neurotherapeutics. When searching Pubmed using the terms “Cerebral  
397 organoid”, “Brain organoid”, “CNS organoid” and “Cortical organoid” the number of  
398 publications for the year 2013 were 4, compared to 52 and 77 for the years 2017 and 2018,  
399 respectively. Due to the significant expansion and importance of this technology, this section  
400 of the review will primarily focus on the applications and advancements in this field. Cerebral  
401 organoids are indeed a relatively new platform but are finding wider application as *in vitro*  
402 disease modelling tools, not only for many developmental disorders, but also for psychiatric  
403 diseases and neurodegenerative conditions (Lancaster et al., 2013; Mariani et al., 2015; Garcez  
404 et al., 2016; Jo et al., 2016; Kelava and Lancaster, 2016a; Raja et al., 2016; Bershteyn et al.,  
405 2017; Birey et al., 2017; Iefremova et al., 2017). The advent of genome editing techniques such

406 as CRISPR/Cas9 has changed the scene for tackling genetic disorders and opened a new  
407 chapter for potential stem cell applications in the clinic (Waddington et al., 2016). In particular,  
408 organoids' versatility and adaptability to genome editing techniques or gene therapy  
409 approaches make them valuable candidates for the identification and testing of novel  
410 therapeutic approaches (Yin et al., 2016; Gonzalez-Cordero et al., 2018).

### 411 **6.1 Microcephaly**

412 Lancaster *et al.* generated organoids from a patient harbouring a *CDK5RAP2* mutation, and  
413 demonstrated that the organoids from the patient with microcephaly were smaller compared to  
414 a healthy control. This was explained by fewer proliferating progenitors and a premature  
415 differentiation in the disease tissues. The group also demonstrated that the phenotype could be  
416 rescued by inducing the expression of the wild-type gene (Lancaster et al., 2013).

417 Furthermore, cerebral organoids have aided the understanding of microcephaly associated with  
418 neuroinfection with the Zika virus. In the study of Garcez *et al.* human cortical organoids  
419 infected with Zika virus exhibited a 40% decrease in size compared to non-infected controls  
420 (Garcez et al., 2016). An elegant study by Qian *et al.* introduced an innovation in culturing  
421 cerebral organoids through the use of miniaturised spinning bioreactors (the SpinΩ), and the  
422 authors determined that infection of organoids with Zika virus resulted in an increase in  
423 apoptosis with consequent reduction in cell proliferation and a marked sparing of the  
424 ventricular zone (Qian et al., 2016). Another study found that human iPSC-derived cerebral  
425 organoids infected with Zika virus had a decrease in PAX6 expressing progenitors in the  
426 proliferative zones and consequently a decrease in differentiated neurons leading to a  
427 disruption in the cortical plate formation (Cugola et al., 2016). Dang *et al.* found that Zika virus  
428 infection in organoids induced a significant upregulation of Toll-like receptor 3 gene, leading  
429 to apoptosis and dysregulation of neurogenesis (Dang et al., 2016).

### 430 **6.2 Macrocephaly**

431 Li *et al.* demonstrated the recapitulation of macrocephaly in cerebral organoids, by the genetic  
432 ablation of *PTEN* using CRISPR/Cas9. Edited organoids exhibited an activation in AKT  
433 signalling in neural progenitors regulating cortical maturation, resulting in a delay in neuronal  
434 differentiation, an increase in cellular proliferation or radial glia progenitors, and a significant  
435 increment in organoid sizes (Li et al., 2017).

### 436 **6.3 Autistic spectrum disorder**

437 Mariani *et al.* employed iPSCs derived from patients with idiopathic autism spectrum disorder  
438 to generate cerebral organoids; the patient tissues exhibited an overgrowth of neurites and  
439 synapses, in a similar fashion to that observed in post mortem brain investigations of  
440 individuals with autism. The same study observed an increased production of GABA-ergic  
441 inhibitory interneurons in patient organoids, while also identifying an upregulation of *FOXG1*,  
442 thus indicating a correlation between the two observations (Mariani et al., 2015). Using  
443 cerebral organoids combined with monolayer cultures, Mellios *et al.* characterised defects in  
444 neurogenesis associated with MeCP2 deficiency in Rett syndrome, which consisted primarily  
445 in expanded ventricular zones with enhanced PAX6+ ventricle-like structures. In this study,  
446 through the inhibition of miR-199, affected signalling pathways (PKB/AKT and ERG/MAPK)  
447 were rescued and the dysregulations in neural differentiation ameliorated (Mellios et al., 2017).

### 448 **6.4 Miller-Dieker syndrome**

449 Miller-Dieker syndrome, a form of lissencephaly, was modelled using patient-derived iPSCs,  
450 enabling the identification of a stalled mitosis of outer radial glia, thus suggesting that

451 dysfunctions in progenitor cell cycles could be a feature of cortical malformations in the disease  
452 (Bershteyn et al., 2017). Another study identified non-cell autonomous defects in Wnt  
453 signalling associated with Miller-Diekers syndrome (Iefremova et al., 2017).

#### 454 **6.5 Sandhoff disease**

455 Allende *et al.* developed cerebral organoids from iPSCs derived from an infant with Sandhoff  
456 disease and from isogenic controls corrected for the *HEXB* mutation by gene editing. The  
457 authors demonstrated that GM2 ganglioside only accumulated in the disease organoids and  
458 affected organoids displayed an increase in size and cellular proliferation compared to the  
459 isogenic control counterpart (Allende et al., 2018).

#### 460 **6.6 Schizophrenia**

461 In their study examining the association of *DISC1* gene with schizophrenia, Ye *et al.* used  
462 human cortical organoids to demonstrate that *DISC1/Ndel1* interactions regulate mitotic events  
463 in neural stem cells and that a delay in mitosis was observed in organoids derived from a patient  
464 with a *DISC1* mutation (Ye et al., 2017).

#### 465 **6.7 Modelling prenatal and perinatal drug exposure**

466 Cerebral organoids have been used to investigate how the prenatal exposure to substances of  
467 abuse including illegal drugs, alcohol and tobacco affect neurogenesis. A study examining the  
468 exposure of cocaine, demonstrated that cytochrome P450 CYP3A5-mediated oxidative  
469 metabolism was responsible for the developmental abnormalities of the fetal neocortex,  
470 resulting in the inhibition of neuroepithelial progenitor proliferation, premature neuronal  
471 differentiation and a reduction in the cortical plate formation (Lee et al., 2017). Zhu *et al.*  
472 investigated the effects of ethanol exposure in organoids to better understand alcohol-induced  
473 defects in neurogenesis in fetal alcohol syndrome, and were able to identify through a  
474 transcriptome analysis, gene expression alterations in the Hippo pathway and in other genes  
475 including *GSX2* and *RSPO2* (Zhu et al., 2017a). Another study using organoids-on-chip  
476 investigated the effect of nicotine on neural development, demonstrating a disruption in cortical  
477 development in exposed organoids (Wang et al., 2018). The use of organoids for studies on the  
478 effect of drug exposure on embryonic CNS development would not be limited to substances of  
479 abuse, but could also be used in the context of neurodevelopmental toxicity whereby  
480 toxicological profiles of compounds on teratogenicity or neurotoxicity could also be assessed  
481 in the system, such as for the evaluation of the neural teratogenic effect of valproic acid or the  
482 effect of environmental chemicals (Schwartz et al., 2015; Miranda et al., 2018b; Wood et al.,  
483 2018).

#### 484 **6.8 Alzheimer's disease**

485 The limitations of cerebral organoids in recapitulating only early neurogenesis, hinders their  
486 application for studying late-onset neurodegenerative diseases such as Alzheimer's,  
487 Parkinson's and Huntington's (Kelava and Lancaster, 2016a). Nevertheless, Raja *et al.*  
488 developed cerebral organoids derived from patients with early onset familial Alzheimer's, and  
489 were able to recapitulate the disease phenotype through the demonstration of  $\beta$ -amyloid  
490 aggregation, hyperphosphorylated tau proteins and abnormal endosomes. The authors further  
491 demonstrated that  $\beta$ -amyloid and tau pathologies were significantly reduced when treating  
492 patient organoids with  $\beta$  and  $\gamma$  secretase inhibitors (Raja et al., 2016).

#### 493 **7. Other developments and applications**

494 More recently, research groups have sought to optimise and advance methods for the  
495 generation of more reproducible and morphologically complex organoids. For instance,  
496 Basuodan *et al.* have generated 3-D cultures with characteristics similar to cerebral organoids  
497 by transplanting iPSC-derived neurospheres embedded in ECM matrix, into brains of  
498 ischaemic mice (Reem *et al.*, 2018).

499 Organoids also provide a powerful tool for the study of evolutionary developmental biology,  
500 and for comparing neurogenesis between species *in vitro* (Giandomenico and Lancaster, 2017).  
501 More recently, due to the advancement in gene editing technologies, such as CRISPR/Cas9,  
502 Neanderthal cerebral organoids were generated by introducing the Neanderthal gene *NOVA1*  
503 in human iPSCs. This study demonstrated that Neanderthal brain organoids resembled to a  
504 certain degree, organoids generated from patients with autism, indicating that these similarities  
505 may be linked to socialisation behaviours (Cohen, 2018).

506 Moreover, organoids have been used to study cellular migration, cross-talk and circuitry  
507 assembly by either generating region-specific organoids and fusing them, or by co-culturing  
508 cells from different lineages in a single organoid, and thus generating structures referred to as  
509 assembloids (Birey *et al.*, 2017; Workman *et al.*, 2017; Pham *et al.*, 2018). By using this  
510 approach, forebrain assembloids derived from patients with Timothy syndrome, were shown  
511 to have defects in the migration of cortical interneurons, and these could be restored  
512 pharmacologically by modulating the mutated L-type calcium channel, thus contributing  
513 significantly to the understanding of epilepsy and autism associated with the syndrome (Birey  
514 *et al.*, 2017).

515 The substantial versatility of organoid applications is demonstrated in the interesting  
516 experiment conducted by Mattei and colleagues, where cerebral organoids were employed to  
517 investigate how neurogenesis and neural development could be affected by microgravity. In  
518 projection of spaceflight advancements, the authors cultured human organoids in rotary cell  
519 culture system to demonstrate that microgravitational changes influenced the expression of  
520 rostral-caudal patterning genes and cortical markers (Mattei *et al.*, 2018).

521 Literature reports on the ability of organoids to recapitulate the composition of an adult CNS  
522 were elusive in the initial phases. Seminal studies on the comparison of cerebral organoids to  
523 fetal brains, initially suggested that the development of fully matured cerebral organoids could  
524 only parallel the early embryonic cerebral development observed at 8-10 weeks gestation  
525 (Mariani *et al.*, 2012; Kelava and Lancaster, 2016a; Kelava and Lancaster, 2016b). However  
526 single cell sequencing experiments have revealed that organoids are capable of replicating late-  
527 mid fetal periods of a 19-24 weeks gestational brain (Pasca *et al.*, 2015).

528 Given the ability of organoids to recapitulate developmental timing, much interest has also  
529 been directed at the types of CNS neural cell populations which compose organoids and their  
530 maturation stage, such as glial cells. A recent study conducted by Monzel *et al.* (2017) reported  
531 the presence of differentiated glial cells in midbrain organoids from as early as day 27 of  
532 development, with myelinating oligodendrocytes ensheathing neurites at day 61 (Monzel *et al.*,  
533 2017). Moreover, the same study demonstrated that after 61 days, mature astrocytes staining  
534 for S100 $\beta$  and AQP4 characterised mature midbrain organoids (Monzel *et al.*, 2017).  
535 Additional studies have further demonstrated that cerebral organoids cultured for prolonged  
536 periods, ranging from months up to 1.5 years, displayed the presence of differentiated  
537 astrocytes and oligodendrocytes (Camp *et al.*, 2015; Renner *et al.*, 2017; Matsui *et al.*, 2018).  
538 Furthermore, using culture times of over a year has been shown to yield organoids exhibiting  
539 a large proportion of mature glial cells and gene expression profiles comparable to those of  
540 post-natal brains (Renner *et al.*, 2017; Sloan *et al.*, 2017).

541 Our group has used cerebral organoids to model mitochondrial neurogastrointestinal  
542 encephalomyopathy (MNGIE), a rare metabolic disorder which manifests with  
543 leukoencephalopathy amongst other neurological and gastrointestinal symptoms (Pacitti, 2018;  
544 Pacitti and Bax, 2018). The ability of organoids to produce differentiated astrocytes and  
545 myelinating oligodendrocytes, and most importantly the recreation of a physiologically  
546 relevant cross-talk between cells has been a great asset for investigating the leukodystrophic  
547 manifestations of the disease and shed light on the poorly understood pathomolecular  
548 mechanisms of the CNS involvement in MNGIE (Pacitti, 2018; Pacitti and Bax, 2018).

549 In comparison to 2-D cultures, brain organoids represent a valuable tool for the study of glial  
550 cells as, for instance, when dealing with astrocytes, traditional monolayer cultures are  
551 inadequate since the morphological complexity and the vast heterogeneity cannot be  
552 appropriately modelled (Imura et al., 2006; Lange et al., 2012; Puschmann et al., 2013). Also,  
553 astrocytes cultured in 2-D preferentially interact with plastic surfaces rather than between cells  
554 and the ECM (Paşca, 2018). Most importantly, astrocytes in 2-D cultures tend to have an  
555 undesirably high baseline reactivity, possibly caused by serum components, although this can  
556 be minimised by using serum-free neurobasal formulations (Foo et al., 2011; Pekny and Pekna,  
557 2014; Pasca et al., 2015). However, iPSC-derived astroglial cells in 2-D cultures require  
558 extensive timing to allow for maturation, and thus practicalities inherent to long term culturing  
559 of cell monolayers, for appropriate astrocyte maturation, represent a major challenge (Dezonne  
560 et al., 2017; Sloan et al., 2017). In addition to cell intrinsic properties, astrocyte maturation  
561 may require interactions with other neural cells types, which would not be represented in pure  
562 astrocyte cultures differentiated by pluripotent cells, unless specifically co-cultured after  
563 differentiation (Chandrasekaran et al., 2016).

564 Three dimensional cultures, like cerebral organoids, allow the recreation of a more  
565 physiological spatial environment that favours a representative organisation of astrocytes and  
566 their interactions with other neural cells and ECM components (Pasca et al., 2015; Liddelw  
567 and Barres, 2017). Compared to 2-D cultures, 3-D cultures have indeed demonstrated a better  
568 capacity for recapitulating astrocyte heterogeneity (Puschmann et al., 2013; Puschmann et al.,  
569 2014; Liddelw and Barres, 2017). Moreover, in 3-D cultures, basal reactivity of astrocytes is  
570 negligible, rendering them the ideal platform for the study of the heterogeneous spectrum of  
571 astrocyte subtypes and their activation (Puschmann et al., 2013; Pasca et al., 2015; Liddelw  
572 and Barres, 2017).

## 573 **8. Current caveats and advancement in the organoid technology**

574 While cerebral organoids offer an advantageous culture system with diversified neural cells for  
575 modelling as closely as possible the intercellular interactions during organogenesis, the  
576 technology also suffers from some limitations, which are constantly being addressed with  
577 ongoing research efforts. One of the greatest limitations of the 3-D platform is the confounding  
578 batch variability (Di Lullo and Kriegstein, 2017; Paşca, 2018). Cell differentiation relies on  
579 spontaneous events that are characterised by a high degree of stochasticity as they lack  
580 developmental axes (Paşca, 2018). This results in regional identities that could differ in  
581 distribution, composition and densities between organoids, generating concerns regarding  
582 reproducibility, accuracy and scalability (Di Lullo and Kriegstein, 2017). The spontaneous self-  
583 patterning mechanisms on which cerebral organoids rely, results in the formation of several  
584 brain regional identities, when compared to brain region-specific organoids. As such, cerebral  
585 organoids are characterised by a great level of heterogeneity and complexity, which result in  
586 morphological variabilities between and within organoid batches, leading to inherent  
587 reproducibility issues (Lancaster et al., 2013; Kelava and Lancaster, 2016a). Referring to this  
588 elevated variability, Lancaster *et al.* (2014) suggested that if using organoids to detect

589 phenotypes in the context of genetic disorders, defects must be robust enough to be noticeable  
590 (Lancaster and Knoblich, 2014; Kelava and Lancaster, 2016b; Giandomenico and Lancaster,  
591 2017). In fact, organoid variability could have severe implications with respect to disease  
592 modelling, drug screening or neurodevelopmental studies, as the heterogeneity could affect the  
593 consistency of phenotypes exhibited, masking true differences between diseased and healthy,  
594 or treated and non-treated tissues. Organoid variability would appear to be partly accountable  
595 to a bioreactor-based effect, meaning that a more controlled growth microenvironment would  
596 contribute to a better reproducibility (Quadrato et al., 2017).

597 More recently, polymer microfilaments were implemented as scaffolds to promote a more  
598 elongated generation of embryoid bodies, which has been found to enhance neuroectoderm  
599 formation and cortical development, and also reduce the issues of reproducibility and  
600 variability observed in the regional identities of filament scaffolded organoids (Lancaster et al.,  
601 2017).

602 Contrarily to the “intrinsic” self-patterning protocol, patterning of organoids using inductive  
603 signals and optimised bioreactors, as conducted by Qian *et al.*, led to the development of more  
604 consistent region specific organoids which were less influenced by batch variability (Qian et  
605 al., 2016). Optimal patterning and the relevant reproduction of proper developmental axes  
606 requires a spatiotemporally defined gradients of morphogens, which is challenging to achieve  
607 in culture; it has been suggested that a way to circumvent this could be through the use of slow-  
608 releasing microbeads to establish a morphogen gradient (Lee et al., 2011; Sun et al., 2018). In  
609 contrast, a recent study revealed that the removal of inductive factors such as those used for  
610 the dual SMAD inhibition during the EB differentiation stage, or refraining from using  
611 maturing growth factors in culture medium during the organoid stage (such as BDNF, GDNF  
612 and TGF- $\beta$ ), yields more optimal organoids with reduced inter and intra batch variability in  
613 terms of reproducibility, size, growth and neural cell composition and maturity (Yakoub and  
614 Sadek, 2018). Cerebral organoids generated through this optimised protocol exhibited a robust  
615 neuronal zone and positive staining for general neuronal and mature astrocytic markers, and  
616 were characterised by a strong upregulation of neurotransmitter receptor genes involved in  
617 synaptic functions including the glutamate,  $\alpha$ -amino-3-hydroxy-5-methyl-4-  
618 isoxazolepropionic acid (AMPA) receptor GluA1, and the N-methyl-D-aspartate (NMDA)  
619 receptors GluN1, GluN2A and GluN2B, and the  $\gamma$ -amino butyric acid (GABA) receptor  
620 GABA-B receptor 1 (Yakoub, 2019).

621 Potentially, the elevated variability observed in EB preparations may contribute to the  
622 heterogeneity observed between organoid preparations (Wilson et al., 2014). Therefore,  
623 controlling this heterogeneity, deriving from the spatial disorganisation and asynchronous  
624 differentiation of EB aggregates, could further minimise reproducibility issues observed during  
625 organoid development (Miranda et al., 2015; Miranda et al., 2018a). The use of centrifugal  
626 forced-aggregation and silicon micro-textured surfaces improved symmetry, size and  
627 synchronised differentiation in EB, increasing consistency between preparations (Ungrin et al.,  
628 2008). Another example of a possible bioengineering solution to control aggregate size and size  
629 by cellular confinement, could be identified in the use of microfabrication technologies where  
630 organoids cultured on a micropillar array exhibited robust brain regionalization and cortical  
631 organisation (Zhu et al., 2017b).

632 Organoids lack some cells of the CNS including endothelial cells composing the cerebral  
633 vasculature, the blood-brain barrier (BBB), and microglia, as these do not derive from  
634 ectodermal tissues (Di Lullo and Kriegstein, 2017). These cells are found to have a role in CNS  
635 development via extrinsic signals that induce maturation and differentiation of neural cells



636 including astrocyte and cortical neurons (Stubbs et al., 2009; Cunningham et al., 2013; Sloan  
637 et al., 2017).

638 The lack of vascularisation has been reported to prevent the delivery of oxygen and small  
639 molecules deep inside the tissue, often resulting in necrosis within the centre of the organoids.  
640 Most importantly, the lack of vascularisation interferes with certain patterning cues necessary  
641 for organoid development and progenitor differentiation. Late developing brains are highly  
642 dependent on vascularisation as niches of neural progenitors, such as the SVZ, are generally  
643 found in proximity of vessels. The solution to the limitations inherent to vascularisation and  
644 stochastic patterning cues can only be sought by refinement of the existing protocols, by either  
645 modifying culture conditions to mimic the physiological environment as closely as possible or  
646 through bio-engineering innovation to provide a flowing system of nutrients to organoids to  
647 reproduce vascularisation (Kelava and Lancaster, 2016a).

648 Recently, it has been suggested that combining organoid culture with microfluidic technology  
649 may circumvent the vascularisation issue, for example, by culturing endothelial cells in  
650 microfluidic channels (Auger et al., 2013) to provide a flow system of nutrients and trophic  
651 molecules, thus allowing the *in vitro* modelling of organoid angiogenesis (Yin et al., 2016).  
652 Having highlighted the lack of vascularisation and BBB as major limitations of cerebral  
653 organoids, it has been envisaged that the introduction of further structural complexities may  
654 enhance the spectrum of applications of this platform (Kelava and Lancaster, 2016a). Several  
655 groups have addressed the lack of the BBB by generating vascularised organoids (Mansour et  
656 al., 2018; Nzou et al., 2018; Pham et al., 2018). Pham *et al.* generated vascularised cerebral  
657 organoids by re-embedding organoids in Matrigel droplets, seeded with iPSC-derived  
658 endothelial cells (Pham et al., 2018). Mansour *et al.*, employed a different approach and  
659 achieved the vascularisation of human organoids, through engraftment in murine cortices *in*  
660 *vivo*. This demonstrated the feasibility of integration with the host, an improvement in viability  
661 and longevity of the tissue, a synaptic connectivity of transplanted organoids and the host, and  
662 ultimately, the formation of a microvascular network in the grafted organoids (Mansour et al.,  
663 2018). Also, Nzou *et al.* generated a six cell type cortical organoid consisting of astrocytes,  
664 pericytes, oligodendrocytes, neural stem cells and vascular endothelial cells, creating a  
665 functional BBB expressing tight and adherent junctions to examine barrier permeability using  
666 neurotoxic compounds (Nzou et al., 2018).

667 The structural complexity of cerebral organoids has its pros and cons. Whereas the high degree  
668 of neural cell diversity and complex cross-talks are an advantage, this may also represent a  
669 disadvantage when trying to test hypotheses related to the contribution of individual cell types  
670 to mechanistic processes. The complementation of a 3-D model with a 2-D cell culture system  
671 of purified cells of interest from the organoids would allow the compartmentalisation and  
672 investigation of individual neural cell types, enabling molecular mechanisms intrinsic to  
673 specific cell types to be teased out.

674

## 675 **9. Concluding remarks**

676 Studies of neural development and neurodegenerative diseases present many challenges due to  
677 the structural and functional complexity of the CNS, together with the limited possibility of *in*  
678 *vivo* experimental manipulation. Although animal models have contributed to the current  
679 knowledge, there are significant structural, cellular and molecular differences in the CNS of  
680 animal and humans, making data extrapolation and interpretation a formidable task. The past  
681 hundred years have seen the evolution of a number of culture systems for modelling the human  
682 CNS. Tissue explants and organotypic cultures were replaced by 2-D cultures thereby

683 permitting investigation in more controlled systems. Issues of tissue availability were  
684 addressed by the development of human neural cell lines derived from tumours and more  
685 recently, the discovery of neural stem cells has permitted the generation of neuronal and glial  
686 cells in large quantities. Three-dimensional culture systems (organoids) are the most recent  
687 technological development in CNS modelling and bridge the gap between native tissue and 2-  
688 D cell cultures. Many advancements have been made in CNS organoid development, as  
689 evidenced by the ability of culturing for prolonged times, the potential to recapitulate late brain  
690 developmental milestones and *in vivo* transplantation. However, ethical and epistemological  
691 issues have been raised around organoids questioning their potential for developing  
692 consciousness (Lavazza and Massimini, 2018; Shepherd, 2018). At present, organoids can only  
693 recapitulate early stages of development and can be used in a relatively narrow spectrum of  
694 applications. However, their use is currently not free of hindrances and thus continuous efforts  
695 must be made for further improvement to overcome their limitations for a more appropriate  
696 and reliable use. One of the major improvements can be found in organoids-on-chip, which as  
697 opposed to traditional organoids, are not self-assembled but are rather constructed to produce  
698 a more reliable and consistent culture, through the inclusion of engineered elements such as  
699 biosensors and microfluidic channels (Tachibana, 2018). At present, the excitement for this  
700 technology is driving elegant research worldwide and it holds the potential for promising and  
701 revolutionary applications.

702

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704

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1533 **Figure 1. Process of neurogenesis**

1534 The CNS originates from the ectoderm layer of the trilaminar germ disc. The process of  
1535 neurogenesis begins with the formation of the neuroepithelium from the neuroectoderm, giving  
1536 rise to the neural tube in a process called primary neurulation (Johns, 2014). The trilaminar  
1537 germ layer disc is composed of the three germ layer tissues, the endoderm, mesoderm and  
1538 ectoderm. The mesoderm gives rise to the notochord, a tubular mesodermal structure which on  
1539 releasing trophic factors, triggers neural induction, whereby uncommitted or naïve ectoderm  
1540 becomes committed to the neural lineage, and subsequently stimulates the formation of the  
1541 neural tube in the overlying ectoderm (Dickinson et al., 1995). As the ectoderm acquires a  
1542 neuroectoderm identity, it forms a fold, initially giving rise to the neural plate and subsequently  
1543 forms the neural fold. The grooves at either side of the fold are called the neural crest. The crest  
1544 then detaches from the margins of the neural fold giving rise to the peripheral nervous system.  
1545 The neural plate continues to fold on itself giving rise to the hollow neural tube; the lumen of  
1546 the neural tube is called neural canal. As the neural tube closes, it forms a fluid filled cavity  
1547 that generates the ventricular zone, an area occupied by progenitor cells such as neuroblasts  
1548 and glioblasts (Johns, 2014; Brodal, 2016; Kelava and Lancaster, 2016a). In the transverse  
1549 section of the neural tube the VZ, intermediate zone and subventricular area can be seen. In the  
1550 VZ mitosis takes place generating radial glia during neurogenesis.

1551 **Figure 2. Evolution timeline of CNS modelling**

1552 The timeline illustrates the evolution from organ explants to the use of 2-D neural cell lines,  
1553 and subsequently a shift towards pluripotent stem cell derived neural cultures leading to the  
1554 development of CNS specific organoids. For each category of modelling a time excursus is  
1555 presented chronologically over 100 years.

1556 **Figure 3. iPSC derivation and characterisation**

1557 The ectopic overexpression of the transcription factors *OCT3/4*, *KLF4*, *SOX2*, *L-MYC*, *LIN28*,  
1558 known to be expressed in embryonic stem cells, reverts mature somatic cells such as dermal  
1559 fibroblasts and peripheral blood mononuclear cells (PBMC) to display a pluripotent  
1560 embryonic-like phenotype (Takahashi et al., 2007; Okita et al., 2013). Transfection of cells with  
1561 vectors expressing these transcription factors enables the epigenetic reprogramming of cells,  
1562 through a series of stochastic events, to express endogenous OCT4 and NANOG, the  
1563 characteristic transcription factors determining the pluripotency, self-renewal and proliferative  
1564 capacity of cells (Lohle et al., 2012). In synergy, the ectopic overexpression of these genes  
1565 triggers a sequence of epigenetic modifications leading to DNA demethylation and chromatin  
1566 changes that eventually result in the acquisition of a pluripotent state in transfected cells  
1567 (Jaenisch and Young, 2008).

1568 A multitude of vectors have been used to deliver the reprogramming factors and these  
1569 approaches are broadly divided into non-viral and viral, and integration and non-integration  
1570 methods. For instance, reprogramming could be achieved using viral vectors including  
1571 retroviruses, lentiviruses and more recently Sendai non-integrating virus. Alternatively, non-

1572 viral methods include mRNA or protein delivery or transient expression achieved with  
1573 episomal plasmids. Pluripotent stem cells are defined by the presence of specific markers  
1574 including cell surface proteoglycans (TRA-1-60 and TRA-1-81) and glycosphingolipids  
1575 (SSEA-3 and SSEA-4) and the expression of transcription factors OCT4 and SOX2 (Thomson  
1576 et al., 1998; Tonge et al., 2011). The resulting pluripotent cells, have the same embryonic  
1577 plasticity for differentiating into almost any tissue type of the three germ layers (endoderm,  
1578 mesoderm and ectoderm) when stimulated by the appropriate signalling molecules and growth  
1579 factors (Itskovitz-Eldor et al., 2000; Okita et al., 2013). Examples of cells derived from the  
1580 germ layers include nervous and epidermal tissue from the ectoderm, haematopoietic and  
1581 muscle cells from the mesoderm, and pancreatic cells from the endoderm.

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1583 2018.

#### 1584 **Figure 4. Different brain regional identities recapitulated by CNS organoids**

1585 The diagram summarises the various patterning methods developed to generate region specific  
1586 CNS organoids. Copyright permission was obtained for the reproduction of images taken from  
1587 Lancaster *et al.* 2013, Jo *et al.* 2016, Qian *et al.* 2016, Pasça *et al.* 2015, Muguruma *et al.* 2015  
1588 and Sakaguchi *et al.* 2015.

#### 1589 **Figure 5. Cerebral organoid formation**

1590 Cerebral organoids originate from pluripotent stem cell derived embryoid bodies cultured in  
1591 low concentrations of bFGF-2 and with ROCK inhibitors to prevent anoikis. The embryoid  
1592 bodies are differentiated towards neuroectoderm, resulting in the formation of neurospheres,  
1593 which are embedded into Matrigel hydrogel droplets. After the embedding, budding  
1594 neuroepithelia generate fluid filled cavities reminiscent of ventricles. The neuroepithelium  
1595 begins to migrate outwardly to generate the cortical layers consisting of Cajal-Retzius cells,  
1596 deep and superficial cortical progenitors. On exposure to retinoic acid, cerebral organoids self-  
1597 organize through self-patterning mechanisms to display diverse populations of neural  
1598 progenitors including radial glia, which expand forming cerebral structures (Lancaster and  
1599 Knoblich, 2014). The region in which radial glia originate, recapitulates the *in vivo* VZ and  
1600 SVZ (Kelava and Lancaster, 2016a). Prior to neurogenesis, radial glia are formed from the  
1601 neuroepithelial cells and facilitate the migration of the neural and glial progenitors (Howard et  
1602 al., 2008; Johns, 2014); these cells are characterised by the asymmetric self-renewal division  
1603 leading to the generation of one neuron and one radial glia (Gotz and Huttner, 2005; Lancaster  
1604 and Knoblich, 2012). Radial glia migrate, establishing the SVZ, where cells divide  
1605 symmetrically forming intermediate progenitors (Haubensak et al., 2004; Miyata et al., 2004).  
1606 Radial glia produce outer radial glia in the SVZ, which are self-renewing (Fietz et al., 2010;  
1607 Hansen et al., 2010). Radial glia residing in the VZ divide at the apical surface adjacent to the  
1608 ventricle. Intermediate progenitors and basal radial glia migrate basally to the SVZ. Neurons  
1609 formed from radial glia, migrate radially from the ventricular and SVZ toward the basal region  
1610 to establish the cortical plate (Johns, 2014; Kelava and Lancaster, 2016a). The neuronal  
1611 migration depends on a layer of Cajal-Retzius cells and the outward migration is regulated by  
1612 the protein reelin secreted by the latter cells (Frotscher, 1998). Within the intermediate zone of

1613 the cerebral hemispheres, neurons undergo apoptosis, and the region becomes the subcortical  
1614 white matter (Johns, 2014).

1615 **Figure 6. Frequency of publications reporting the use of CNS organoids by year**

1616 The chart illustrates a surge in publications involving the use of CNS organoids, between 2014-  
1617 2018.

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In review

1625 **Table 1. Summary of different CNS neural cells differentiated from iPSC**

1626 Neural cells characteristic of the CNS have been generated by directed differentiation of pluripotent stem cell derived lines, to recapitulate specific  
 1627 cell types or disease condition.

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Disease group	Disease modelled	Genetic/chromosomal abnormality	iPSC-derived cells	Reprogramming method	Reference
<b>Lysosomal storage disorders</b>	Jansky-Bielschowsky disease	<i>CLN5</i>	CLN5 neurons	Sendai-virus transduction	(Uusi-Rauva et al., 2017)
	Batten disease	<i>CLN3</i> , <i>TPP1</i>	CLN3 neurons	Retrovirus transduction	(Lojewski et al., 2014)
	Pompe disease	<i>GAA</i>	Pompe neurons	Retrovirus transduction	(Higuchi et al., 2014)
	Niemann-Pick type C1	<i>NPC1</i>	NPC1 neurons, astrocytes	Retrovirus transduction; lentivirus transduction	(Trilck et al., 2013) (Efthymiou et al., 2015)
<b>Metabolic disorders</b>	Lesch-Nyhan syndrome	<i>HPRT</i>	Neurons	Retrovirus transduction	(Mastrangelo et al., 2012)
	Gaucher's disease	<i>GBA1</i>	Dopaminergic neurons, neurons	Lentivirus transduction	(Panicker et al., 2012) (Tiscornia et al., 2013) (Awad et al., 2015) (Sun et al., 2015)
	Metachromatic leukodystrophy	<i>ARSA</i>	Neural stem cells, astroglial progenitor cells	Retrovirus transduction	(Doerr et al., 2015)
	X-linked Adrenoleukodystrophy	<i>ABCD1</i>	Neurons, astrocytes, oligodendrocytes	Retrovirus transduction; lentivirus transduction	(Jang et al., 2011) (Baarine et al., 2015)
<b>Neurodegenerative Disorders</b>	Parkinson's disease (PD); idiopathic PD	<i>LRRK2</i> ; ?	Midbrain dopaminergic neurons	Cre-recombinase excisable viruses; retrovirus transduction	(Soldner et al., 2009) (Nguyen et al., 2011) (Sanchez-Danes et al., 2012) (Fernandez-Santiago et al., 2015)

	Amyotrophic lateral sclerosis (ALS)	<i>TDP-43;</i> <i>SOD1</i>	Spinal motor neurons, astrocytes	Retrovirus transduction; TALEN transfection; sendai-virus transduction, episomal transfection	(Bilican et al., 2012) (Egawa et al., 2012) (Serio et al., 2013) (Yang et al., 2013) (Bhinge et al., 2017)
<b>Neurodevelopmental disorders</b>	Rett syndrome	<i>TRPC6;</i> <i>MECP2</i>	Neural progenitor cells, glutamatergic neurons, astrocytes	Retrovirus transduction	(Muotri et al., 2010) (Marchetto et al., 2010) (Ananiev et al., 2011) (Kim et al., 2011) (Williams et al., 2014) (Djuric et al., 2015) (Griesi-Oliveira et al., 2015) (Tang et al., 2016)
	Atypical Rett syndrome	<i>CDKL5</i>	Glutamatergic neurons, GABAergic neurons	Lentivirus transduction; Retrovirus transduction;	(Amenduni et al., 2011) (Ricciardi et al., 2012)
	Timothy syndrome	<i>CACNA1C</i>	Neural progenitor cells, cortical glutamatergic neurons	Retrovirus transduction	(Pasca et al., 2011) (Tian et al., 2014)
	Down Syndrome	Trisomy 21	Cortical glutamatergic neurons	Lentivirus transduction	(Shi et al., 2012a)
	Familial dysautonomia	<i>IKBKAP</i>	Neural crest precursors	Lentivirus transduction	(Lee et al., 2009; Lee et al., 2012)
	Fragile X Syndrome	<i>FMR1</i>	Neural progenitor cells, forebrain neurons, glial cells	Retrovirus transduction; episomal transfection	(Urbach et al., 2010) (Doers et al., 2014) (Park et al., 2015) (Halevy et al., 2015)
	Cockayne syndrome	<i>ERCC6</i>	Neural progenitor cells	Sendai-virus transduction	(Vessoni et al., 2016)
	Angelman/Prader-Willi syndromes	<i>UBE3A</i>	Neurons, astrocytes	Retrovirus transduction	(Chamberlain et al., 2010)
	Phelan-McDermid syndrome	22q13 deletion	Forebrain neurons	Retrovirus transduction	(Shcheglovitov et al., 2013)

<b>Neuropsychiatric Diseases</b>	Frontotemporal dementia (FTD)	<i>CHMP2B</i> ; <i>C9ORF72</i>	Forebrain cortical neurons	Retrovirus transduction; episomal transfection	(Almeida et al., 2013) (Zhang et al., 2017)
<b>Epilepsy</b>	Dravet syndrome	<i>SCN1A</i>	Dopaminergic, GABAergic, glutamatergic neurons; forebrain interneurons, glial cells	Retrovirus transduction	(Higurashi et al., 2013) (Jiao et al., 2013) (Liu et al., 2013; Liu et al., 2016)
	Early infantile epileptic encephalopathy	<i>STXBP1</i>	GABAergic, glutamatergic neurons	Episomal transfection	(Yamashita et al., 2016)
<b>Neuromuscular disorders</b>	Spinal muscular atrophy (SMA)	<i>SMN1</i>	Forebrain, sensory, motor neurons, astrocytes	Lentivirus transduction; retrovirus transduction; episomal transfection	(Ebert et al., 2009) (Chang et al., 2011) (Sareen et al., 2012) (Corti et al., 2012) (McGivern et al., 2013) (Schwab and Ebert, 2014) (Yoshida et al., 2015) (Boza-Moran et al., 2015) (Ng et al., 2015) (Nizzardo et al., 2015) (Liu et al., 2015) (Fuller et al., 2015) (Xu et al., 2016) (Patitucci and Ebert, 2016)
<b>Movement disorders</b>	Huntington's disease	<i>HTT</i>	Medium spiny neurons	Lentivirus transduction	(The Hd iPsc Consortium, 2012)
	Hereditary spastic paraplegia	<i>SPG3A</i> , <i>SPG4</i> , <i>SPG11</i> ; <i>ATL1</i> ; <i>SPAST</i>	Cortical neural progenitor cells; forebrain, glutamatergic neurons	Lentivirus transduction, episomal transfection; retrovirus transduction	(Denton et al., 2014) (Havlicek et al., 2014) (Zhu et al., 2014) (Mishra et al., 2016)
	Ataxia telangiectasia	<i>ATM</i>	Neural progenitor cells, GABAergic neurons	Lentivirus transduction	(Nayler et al., 2012) (Carlessi et al., 2014)



Friedrich's ataxia

*FXN*

Neural progenitor cells,  
neural crest cells, peripheral  
sensory neurons, glial cells

Retrovirus transduction;  
lentivirus transduction;  
transposon transfection

(Liu et al., 2011)  
(Eigentler et al., 2013)  
(Hick et al., 2013)  
(Bird et al., 2014)

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In review

Figure 1.TIF

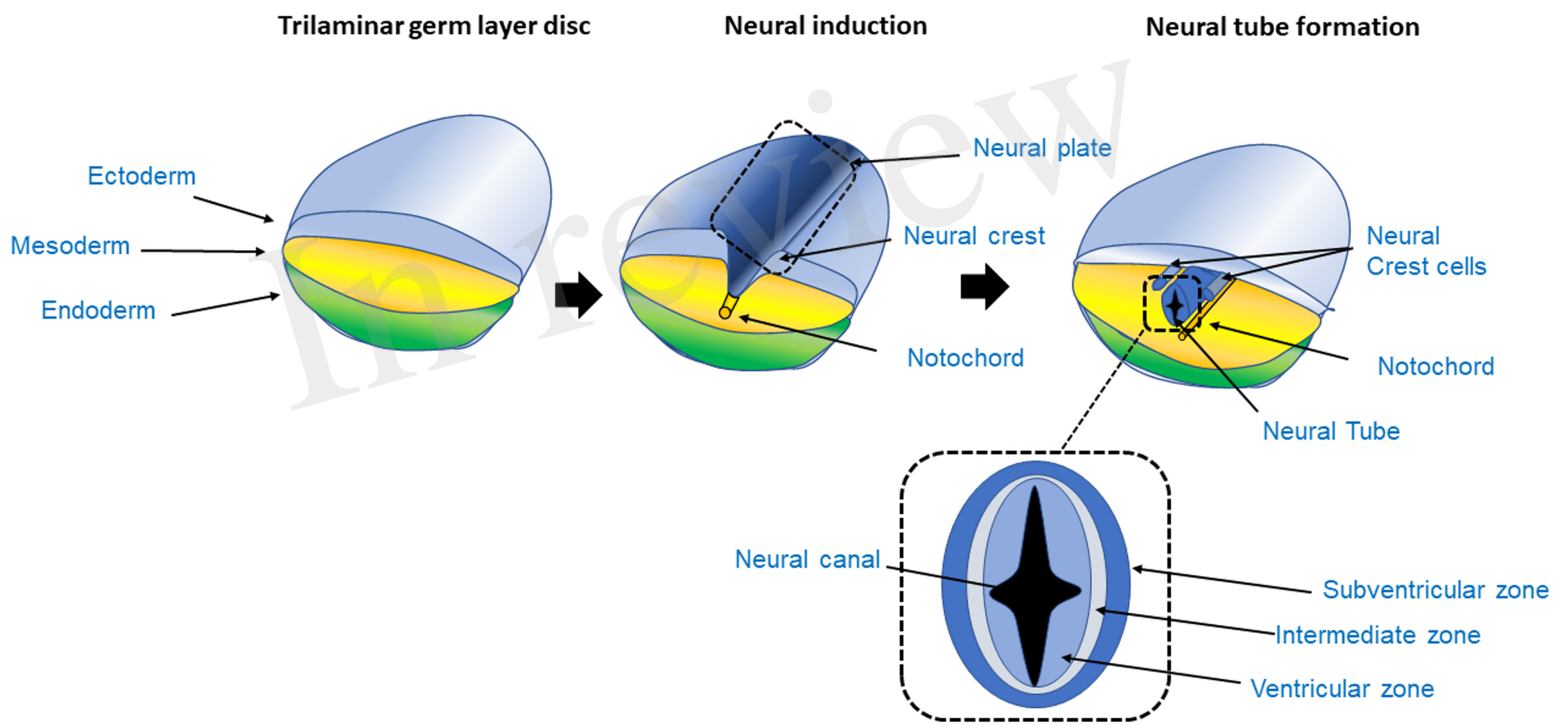


Figure 2.TIF



Figure 3.TIF

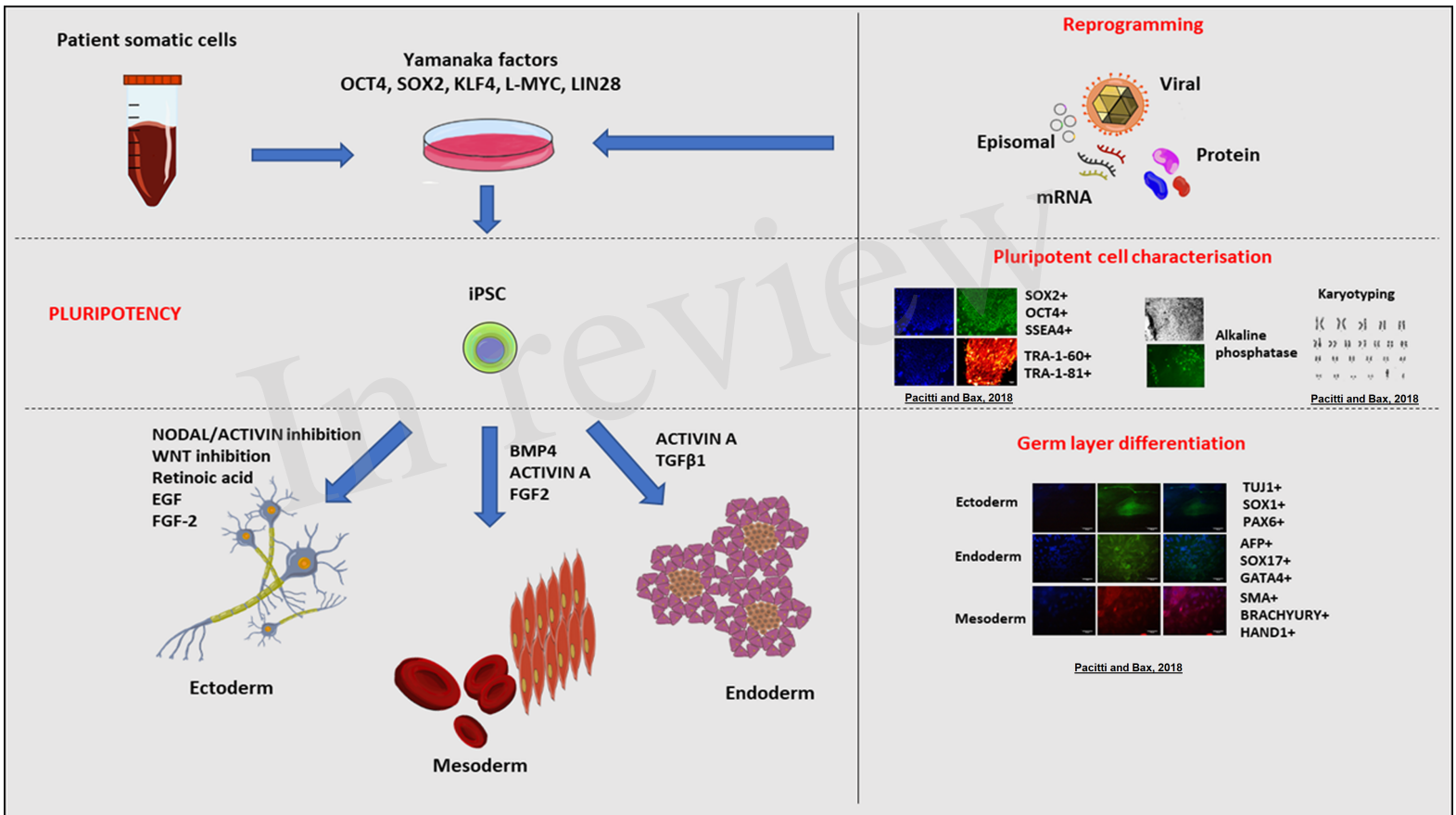


Figure 4.TIF

In review

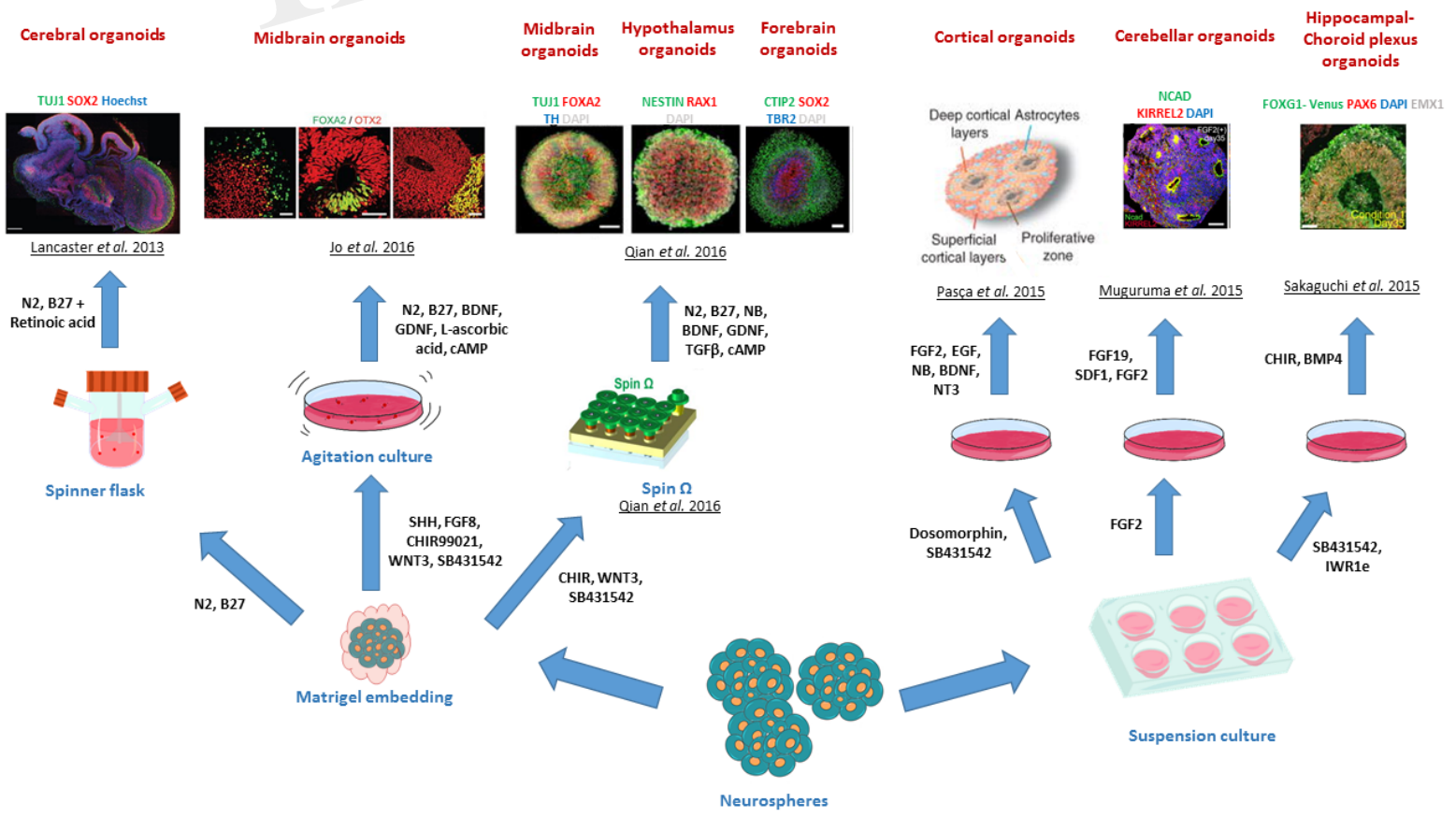


Figure 5.TIF

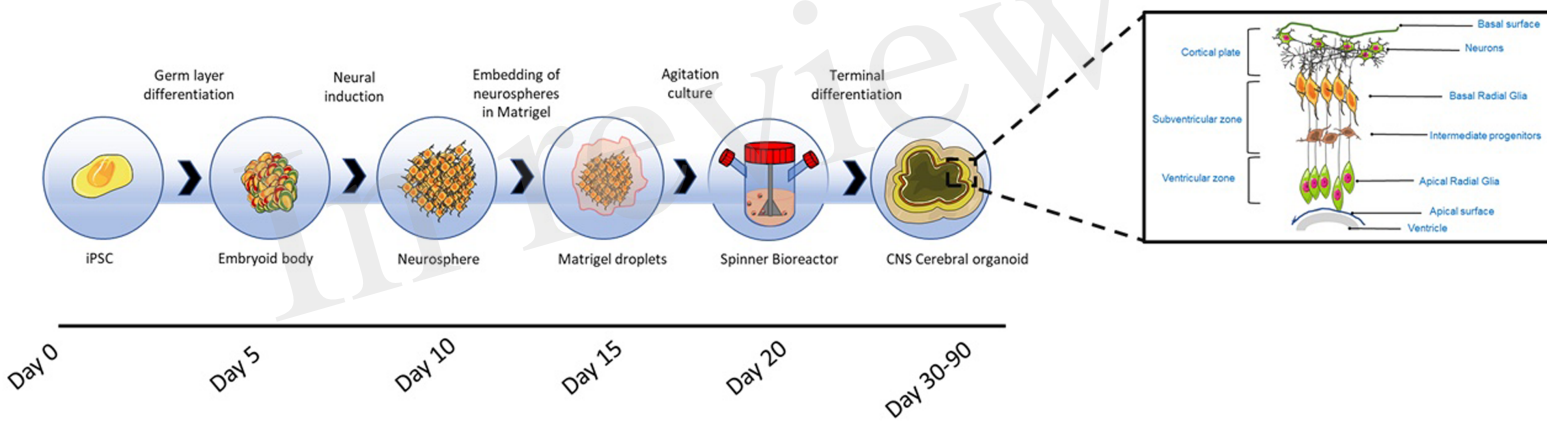


Figure 6.TIF

